

Disrupted salience network dynamics in Parkinson's disease patients with impulse control disorders

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KEYWORDS

Parkinson's disease, impulse control disorders, dynamic functional connectivity, graph theory, salience network.

ABSTRACT

- **Background:** Dynamic functional network analysis may add relevant information about the temporal nature of the neurocognitive alterations in PD patients with impulse control disorders (PD-ICD). Our aim was to investigate changes in dynamic functional network connectivity (dFNC) in PD-ICD patients, and topological properties of such networks.
- **Methods:** Resting state fMRI was performed on 16 PD PD-ICD patients, 20 PD patients without ICD and 17 healthy controls, whose demographic, clinical and behavioral scores were assessed. We conducted a group spatial independent component analysis, sliding window and graph-theory analyses.
- **Results:** PD-ICD patients, in contrast to PD-noICD and HC subjects, were engaged across time in a brain configuration pattern characterized by a lack of between-network connections at the expense of strong within-network connections (State III) in temporal, frontoinsular and cingulate cortices, all key nodes of the salience network. Moreover, this increased maintenance of State III in PD-ICD patients was positively correlated with the severity of impulsivity and novelty seeking as measured by specific scales. While in State III, these patients also exhibited increased local efficiency in all the aforementioned areas.
- **Conclusions:** Our findings show for the first time that PD-ICD patients have a dynamic functional engagement of local connectivity involving the limbic circuit, leading to the inefficient modulation in emotional processing and reward-related decision-making. These results provide new insights into the pathophysiology of ICD in PD patients and indicate that the dFC study of fMRI could be a useful biomarker to identify patients at risk to develop ICD.

1. INTRODUCTION

Impulse control disorders (ICDs), occur in at least 13.6% of patients with Parkinson's disease (PD) on dopaminergic medication. They have been conceptualized as 'behavioral addictions' and are the result of abnormal modulation of the mesocorticolimbic dopamine system [1].

Dopaminergic depletion in PD mainly involves the nigrostriatal 'motor' loop, but also the ventral tegmental area (VTA) projecting to the ventral striatum (VS), amygdala and hippocampus (mesolimbic dopaminergic pathway), and to the orbitofrontal (OFC), frontoinsula, cingulate and prefrontal (PFC) cortices (mesocortical dopaminergic pathway). These regions are critically involved in the modulation of emotional processing, hedonic evaluation and reward-related decision-making [2], all closely associated with ICDs. However, the pathophysiology of ICDs in PD patients is not well understood. Evidence from metabolic [3], functional magnetic resonance imaging (fMRI) [4,5] and morphometric neuroimaging studies [6] has demonstrated abnormalities within the mesocorticolimbic circuit in patients with PD and ICD (PD-ICD) although not always in the same direction and regions [7]. In particular, resting state fMRI (rs-fMRI) studies, have produced controversial results in PD-ICD patients, with both weaker [4] and stronger [8] functional connectivity (FC) detected in cortical areas of the limbic circuit, as well as disrupted functional coupling in brain-wide networks such as the salience, executive and default-mode networks [9,10]. In addition, there have been very few studies into the topological characteristics of brain networks in these patients using graph theory analysis [11,12].

Significantly, most rs-fMRI studies on PD patients have investigated FC patterns as a static phenomenon, while recent evidence shows that FC may vary over time [13]. Such temporal fluctuations can be captured by dynamic functional network connectivity (dFNC) studies [14], providing greater insight into the fundamental properties of brain networks. In PD patients,

temporal fluctuations in FC have been described as closely related to the severity of motor [15] and cognitive impairment [16,17], but its relation with impulsivity has not been studied. Given that previous static FC studies have shown that dopaminergic firing is able to alter limbic cortical signals to the VS, impairing the ability to change behavioral focus in response to change in stimulus salience [8,9,18], a dFNC approach may add relevant information as it represents the temporal changes of these connections [13]. For this reason, we hypothesized that PD-ICD patients would show specific dynamic functional connectivity (dFNC) changes in particular areas of the salience network/reward processing, possibly because these patients may continue to focus on those reward stimuli that have primarily induced the dopamine release, looping the cerebral areas implicated in hedonic evaluation of the stimulus and reward-based decision making. Therefore, the aim of this study was to evaluate differences in dFNC and topological metrics in PD patients with and without ICDs, utilizing a combination of dFNC analyses and graph-theory approaches (GTA) during rs-fMRI.

2. MATERIALS AND METHODS

2.1. Subjects

The final study sample consisted of 62 participants took part from three groups: 20 PD-ICD patients, 22 PD patients without ICD symptoms (PD-noICD) and 20 healthy controls (HC). Participants in each group were matched on age, sex, education and premorbid Intelligence Quotient. All PD patients were diagnosed according to the UK Parkinson's Disease Society Brain Bank criteria and recruited from the Movement Disorders Unit at the Hospital Donostia. A neurologist and a psychiatrist detected and confirmed ICD diagnosis based on the DSM-V and on the Questionnaire for Impulsive-Compulsive Disorders in Parkinson's Disease (QUIP) [19]. ICD severity was scored using the QUIP-Rating Scale (QUIP-RS) [20]. The score of each ICD

subtype in every patient was above the established cut-off value (Supplementary Table 1). We excluded patients with dementia, cognitive impairment following the level II guidelines of the Movement Disorders Society (MDS) Criteria Task Force [21], dyskinesias, previous brain surgery, and patients with past ICD no longer symptomatic. **HCs were recruited from the Basque Center on Cognition, Brain and Language (BCBL) participant pool. They were also evaluated by a neurologist and a psychiatrist and subjects with any neurological or psychiatric disorder were excluded. In addition, based on general population impulsivity scales, HCs with high scores at the higher end of the impulsivity scale were also excluded.** Participants were evaluated using a battery of tests for motor, behavior and cognition (Table 1 and Supplementary Table 2). PD patients were studied under the effect of their usual dopaminergic medication. The study was approved by the Local Ethics Committee and written informed consent was obtained from all subjects prior to their enrollment.

2.2. MRI data acquisition and preprocessing

The rs-fMRI and structural data were acquired on a 3T Siemens Magnetom TIM Trio MRI scanner (Siemens Medical Solutions, Erlangen, Germany) using a 32-channel head coil. Further information on the MRI data acquisition and preprocessing is included in the Supplementary Materials. Briefly, the Conn Functional Connectivity Toolbox v.17.f [22] running on Matlab™ 9.1 (release R2016b) was used to conduct standard preprocessing routines and analyses. **None of the participants included in the study sample had white matter abnormalities in their T2-weighted MRI images.**

2.3. Motion correction

To minimize the potential effects of head movements on dFNC results, we applied stringent inclusion criteria [14] following previous articles published on dFCN in PD populations [15,16]

(see details in Supplementary Text). Briefly, subjects with a mean framewise displacement (FD) > 0.5 mm or with a maximum displacement > 3 mm in translation indexes x, y, or z or $> 3^\circ$ in rotation indexes were excluded from the analysis. Thus, nine participants (4 PD-ICDs, 2 PD-noICDs, 3 HCs) were excluded. In addition, there were no statistical root mean square (RMS) movement differences between PD-ICD (0.1 ± 0.09), PD-noICD (0.08 ± 0.09) and HC (0.12 ± 0.1) groups ($p = 0.47$).

2.4. Identification of intrinsic connectivity networks

The data were decomposed into functional networks by applying a spatial group independent component analysis (ICA) using the Group ICA of the fMRI Toolbox (GIFT v4.0a; <http://icatb.sourceforge.net>). We chose relatively high model order ICA, each individual's functional data was reduced to a total of 134 independent components (ICs) through a principal component reduction and subsequently, the concatenated subject-reduced data was reduced to 100 ICs at the group level using the expectation maximization algorithm [23] included in GIFT.

Of the 100 ICs, 40 were identified as meaningful by two independent reviewers (I.N. and J.K.), based on expectations that resting state networks should exhibit peak activations in gray matter, low spatial overlap with known vascular, ventricular, motion, and susceptibility artifacts, and time-courses dominated by low frequency fluctuations and with a high dynamic range [24]. **Also, to examine potential between-group differences in gray matter we used participants' T1-weighted images to run Freesurfer's mri_glmfit [25] on gray-matter volume, cortical thickness, and surface area. We found no significant differences in any of the group comparisons (PD-ICDs vs. PD-noICDs, PD-ICDs vs. HCs, PD-noICD vs. HCs).**

Using spatial correlation values between ICs and the template [26], we classified the selected components into the following seven functional networks: basal ganglia [BG], auditory [AUD],

sensorimotor [SMN], visual [VIS], cognitive-executive [ECN, including language and salience networks], default mode [DMN] and cerebellar networks (Figure 1A). The cognitive control network included IC components involved in directing and monitoring behavior and in mediating memory and language functions because of their overlap in several areas, as in previous works in the field [27]. Pairwise Pearson's correlations were computed and converted to z-scores using Fisher's z-transformation to create the statistical FNC matrix (Figure 1B and 1C). For further details in identification of intrinsic connectivity networks see Supplementary Text.

2.5. Dynamic functional network connectivity (dFNC) analysis

dFNC was examined using the GIFT toolbox for dynamic FNC applying two approaches: a sliding window approach (changes in FNC across time) and k-means clustering (extracting reoccurring FNC patterns) First, we used a sliding-window approach, in which a sliding time window of the 22-repetition time (TRs) method was applied to each subject, with a Gaussian window alpha value of 3 and a step between windows of 1 TR, resulting in 270 consecutive windows. To promote sparsity in the estimations, a penalty was imposed on the L1 norm of the precision matrix. We also applied a k-means clustering algorithm to the 270 FC window FNC matrices for all the subjects, which was iterated 150 times. To reduce redundancy between windows and computational demands, windows consisting of local maxima in functional connectivity variance were used. In addition, we used the L1 distance for k-means computing to combine similar FC matrices from the different windows. We used age, sex and depression scores as covariates, the latter due to the significant differences between the groups (Table 1). The covariates were included in the clustering algorithm using the GIFT toolbox (<http://icatb.sourceforge.net/groupica.htm>). Based on the elbow criterion of the cluster validity index, the optimal number of clusters was determined to be four ($k = 4$), the so-called states I, II,

III and IV. Using the resultant four cluster centroids, all FNC matrices of each subject were then categorized as belonging to one of the four clusters or states based on their similarity to the cluster centroids. From these data, we obtained a state transition vector and final cluster centroids were obtained as the median of all state-assigned FCN matrices across time. The subject-specific centroid of each state was computed by calculating the median value of each FCN matrix for that state.

We used three different indices to examine the temporal properties of the dFNC states: (1) Fractional window (FW), the proportion of time spent in each state; (2) mean dwell time (DT), represents how long the participant remained in a certain state; (3) the number of transitions, the total number of changes between states. The differences between groups were assessed using an ANOVA, applying a LSD post-hoc test. Moreover, the FC differences between the groups in each FC state were investigated with the network-based statistic (NBS) tool. A p value FDR corrected for multiple comparisons was calculated. The significance of FC differences were tested using an ANOVA test for the three group differences and post-hoc pairwise comparisons. Overall, the p values were false discovery rate (FDR) corrected for multiple comparisons (i.e.: q values). See Supplementary Text for more details about dFNC analysis.

2.6. Graph-theory parameter analysis

Graph characteristics of the networks were analyzed using GRETNA software v 2.0.0 (<http://www.nitrc.org/projects/gretna>) in the FNC configuration. We investigated the topological characterization of brain connectivity, studying local (clustering coefficient, betweenness centrality and the local efficiency) and global (global efficiency and assortativity) metrics. For further details see Supplementary Text.

2.7. Statistical analyses

Statistical methods for clinical variables are detailed in Supplementary Text. The threshold for statistical significance was $p < 0.05$. We used a Pearson's correlation analysis to explore the associations between the temporal properties and the clinical measures in PD-ICD patients, applying a post-hoc Bonferroni correction for multiple comparisons (IBM SPSS Statistics v16.0).

3. RESULTS

3.1. Sociodemographic and clinical data

This analysis was carried out in 16 PD-ICD, 20 PD-noICD patients and 17 HC (nine participants were excluded from the initial sample because of motion criteria). PD-ICD patients had significantly higher novelty seeking personality traits, impulsivity and depression scores than the other groups. There were no other clinical or cognitive differences between the groups (Table 1 and Supplementary Table 2).

3.2. Intrinsic connectivity networks

The spatial maps of the 40 ICs defined were established using the group ICA (see Figure 1 and Supplementary Table 3). Based on their anatomical and presumed functional properties, the ICs were grouped into the following networks: BG (IC 16, 22, 37); AUD (IC 34); SMN (IC 19, 4, 3, 54, 68, 24, 12); VIS (IC 25, 42, 90, 93, 59, 40, 26, 44, 45); ECN (IC 78, 49, 62, 92, 47, 18, 35), encompassing the language (IC 43, 79) and salience networks (IC 85, 39, 56); DMN (IC 15, 23, 88, 48, 66, 76); and the cerebellar network (IC 29, 31).

3.3. Differences in dynamic FC

A k-means clustering algorithm identified four different dFNC matrix centroid configurations or states that were recurrent throughout the rs-fMRI acquisition and across subjects (Figure 2A and 2B). The most frequent state (State III, 45% of acquisition time) appeared as a within-network FC configuration, particularly associated with the SMN, VIS and ECN networks which almost completely lacks between-network connectivity. By contrast, the other three states were more infrequent (State I 16%; State II 19%; State IV 19%), and they displayed between-network FC configurations that included positive correlations between the SMN and VIS networks, as well as anti-correlations between the SMN and DMN, and between the ECN and DMN networks. When the 5% of the FC network with the strongest connections was represented, State III had the most positive within-network coupling (Figure 2C). **In States I, II and IV we observed that 60% of connections were between networks (VIS-SM, SM-cerebellum, VIS-DMN, DMN-SM, ECN-VIS, BG-VIS, BG-ECN, etc.). However, in State III we observed 38 stronger within- and between-network connections of which only 30% were between-network connections. Thus, State III was predominantly characterized by within-network connections (particularly connections between independent components located in the ECN, VIS and SM networks).**

In terms of temporal properties, State III showed a trend to be more frequent (higher FW) in PD-ICD patients (57 ± 0.3) than in the PD-noICD subjects (40 ± 0.3) or the HCs (39 ± 0.2) ($F(2,50) = 2.41$; $p = 0.07$). In parallel, these patients showed a significantly larger mean DT in State III (41.5 ± 20.7) ($F(2,50) = 3.88$; $p = 0.027$), characterized by stronger local connectivity than PD-noICD subjects (24.8 ± 18.9 ; $p = 0.028$) and HCs (21.6 ± 10.5 ; $p = 0.013$; Figure 3.1.; Supplementary Figure 1). There were no differences in transition number. When the FC differences were calculated between the PD-ICD, PD-noICD and HC groups for each dFNC state ($q < 0.05$ FDR corrected; Supplementary Figure 2), we found that the within-network FC of the

saliency network was enhanced in PD-ICD patients in State III, specifically in the superior temporal lobe, frontoinsular and cingulate cortices ($q < 0.05$ FDR corrected).

3.4. Relationship with clinical properties

In PD-ICD patients, only in State III, the mean DT was positively correlated with the TCI-R NS4 sub-score (disorderliness: $r(14) = 0.519$; $p = 0.039$) and with the non-planning sub-score of the BIS scale ($r(14) = 0.541$; $p = 0.030$), and the mean percentage FW was correlated with the non-planning sub-score of the BIS scale ($r(14) = 0.536$; $p = 0.032$) and with the total score of the BIS scale ($r(14) = 0.561$; $p = 0.024$; Figure 3.2). These effects were not observed either in PD-noICD patients, or in HCs ($p \geq 0.25$). In addition, dopaminergic medication ($LEDD_{TOTAL}$ and $LEDD_{DA}$) was not correlated with any temporal property of State III ($p \geq 0.34$).

3.5. Graph topological properties

We found no differences in global network metrics, yet when regional properties were considered. The PD-ICD patients had greater local efficiency than PD-noICD subjects (the average shortest path connecting all neighbors of a node) in the superior temporal lobe (BA 48; saliency network, SAL; $p = 0.0440$), frontoinsular (BA 6; SAL; $p = 0.0384$) and cingulate cortices (BA32; SAL; $p = 0.0160$), all of which belong to the saliency network.

4. DISCUSSION

This is the first study investigating dFNC and graph properties in PD-ICD patients during rs-fMRI. Our results reveal that in contrast to PD-noICD and HC subjects, PD-ICD patients were engaged across time in a brain configuration pattern characterized by a lack of between-network connections at the expense of strong within-network connections (State III) in temporal, frontoinsular and cingulate cortices, all key nodes in the saliency network. Moreover, this

increased maintenance of State III in PD-ICD patients, reflected by its temporal dFNC properties (FW and DT), was positively correlated with impulsivity (BIS scale) and novelty-seeking personality (TCI-R NS) ratings. Importantly, PD-ICD patients also exhibited increased local efficiency in all the aforementioned areas, suggesting brain reorganization in regions responsible for emotional processing and hedonic evaluation and associated with reward-related decision making.

FCs can be classified into long-range connections between different networks (between-network connectivity), allowing integration of long-distance information, and local connections within clusters of neurons (within-network connectivity) favoring local information processing. In our cohort, the dFNC analyses suggested four different connectivity patterns or states. State III was characterized by reduced expression of between-network coupling and a prominent within-network connectivity, mainly in the SMN, VIS and ECN networks. Accordingly, State III could be interpreted as involving a lower degree of connectedness between regions whereas the other (States I, II and IV) showed stronger between-networks couplings.

Few studies have investigated dFNC in PD patients showing higher between-network FNC in PD patients than in HCs, interpreted as a potential compensatory mechanism [15] and reduced links between networks connectivity in PD patients with mild cognitive impairment [16,17]. In our study, PD-ICD patients showed enhanced maintenance (DT) and a tendency towards remaining for higher proportion of time with functional connections (FW) in State III with respect to the other two groups. This confirms our hypothesis that altered temporal properties in dynamic connectivity is associated with ICD in PD patients. Thus, PD-ICD patients gravitate toward configurations with predominantly within-network FNC patterns, characterized by stronger connectivity between critical hubs that make up the salience network responsible for anchoring

awareness through integration of contextual, hedonic, homeostatic and interoceptive processes, and which partially overlaps with regions of the mesocorticolimbic circuit: the superior temporal lobe, and frontoinsula and cingulate cortices. The temporal predominance of this modular brain organization could reflect dopaminergic dysregulation of the emotional processing circuit in PD-ICD patients, in line with a proposed theory linking the relevance of a specific cognitive process to the length of time spent in the state that facilitates this cognitive aspect [28]. This may leave PD-ICD patients permanently focused on rewarded stimuli, an effect primarily due to dopamine overstimulation which leads to abnormal reward weighting. Importantly, our result is especially relevant considering that PD patients with and without ICD had no cognitive differences in any cognitive domain.

In addition, the FW and the DT in state III in PD-ICD patients were positively associated with the BIS scale, which measures different aspects of impulsivity, but also with the Novelty Seeking personality test evaluating exploratory activity in response to novel stimuli, highlighting the specificity of the findings. Accordingly, a recent static FC study demonstrated the presence of a specific pattern of intrinsic connectivity within and between the SAL, ECN and DMN at baseline in drug naïve PD patients who went on to develop ICD after treatment [10]. Our results emphasize the importance of dFNC studies, not only to analyze the pathophysiology of impulsivity in PD-ICD patients but also to assess its relevance in enhancing the drive to seek and explore novel stimuli. Such an effect deserves further study in drug-naïve PD patients, as it is a personality trait that could play a role in the development of ICDs.

Specifically, PD-ICD patients only appear to exhibit stronger local connections and increased local efficiency in areas that belong to the salience network. This is a large-scale limbic-paralimbic network that encompasses cortical areas which play an important role in orienting

attention to integrate salient, hedonic and interoceptive stimuli which facilitate goal-directed behavior, [29] such as the anterior cingulate cortex, bilateral insula, frontoinsula cortex, amygdala, VS, and substantia nigra/VTA [29]. Abnormal connectivity within this network has been associated with substance-related disorders and addictive behaviors, and interestingly, a recent dFNC study on the general population suggested that susceptibility to tempting stimuli is governed by individual differences in salience network dynamics [30].

Graph theoretical methods provide a mathematical framework to study the topological properties of networks, indicating that while global network measures may exhibit greater temporal stationarity, regional network measures may be more susceptible to local cell dynamics [31]. To date, only two studies have reported disruptions in regional topology in PD-ICD patients: one revealed altered properties of connections to the mesocorticolimbic system [12], while the other, demonstrated stable topological properties irrespective of the state of medication [11], which is relevant to our study. dFNC alterations in PD-ICD patients were accompanied by greater local efficiency in the PD-ICD group in areas of the salience network associated with stable global efficiency. Since local efficiency reflects the capacity for regional specialization in a network, it is plausible that dopaminergic treatment in PD-ICD patients specifically drives the functional reorganization of integrated brain networks, enhancing the aberrant coupling and looping of the reward system.

The present study has some limitations. Similar to other studies in the field [9,10], the sample size can be considered relatively small. However, our groups were individually matched for age, sex, education and IQ in order to reduce variability. Although the fact that patients were studied on medication can be considered a limitation, we chose this study design because ICD is a complication associated with dopaminergic treatment. In addition, topological properties are not

affected by medication [11] and dopaminergic medication did not differ between groups or show any association with the temporal properties of dynamic FNC. Finally, even if the duration of the resting state session and the movement threshold might be considered somewhat liberal for studies in healthy populations, we have used the same methodology than studies of dFNC in special populations with neurodegenerative diseases (Alzheimer disease, frontotemporal dementia and PD patients) [15,16].

In conclusion, abnormal temporal patterns and stronger local topological properties in PD-ICD patients suggest a dynamic functional engagement of local connectivity involving the limbic circuit, leading to the inefficient modulation in emotional processing and reward-related decision-making. Moreover, these FNC alterations are not only coupled to impulsivity but also to a strong novelty seeking personality, suggesting that the above-mentioned functional abnormalities contribute to such traits. These findings suggests that a reorganization of the brain occurs in these patients such that regions involved in affection, reward processing and goal-directed behavior acquire a more significant role relative to other neurocognitive processes. We believe this analysis of the temporal dynamics of functional connectivity provide new insights into the pathophysiology of ICD in PD patients and that could be a useful imaging biomarker to identify PD patients at risk to develop ICD.

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Tables and figure legends

Table 1. Sociodemographic, clinical and behavioral characteristics of the sample

	PDICD n=16	PDnoICD n=20	HC n=17	<i>p</i>	Post-hoc (Bonferroni or U Mann Whitney)
Age	61.25 (8.1)	62.45 (8.8)	63.6 (9.9)	0.843 ^a	
Sex, male (%)	14 (87.5%)	16 (84.2%)	14 (82%)	0.834 ^b	
Education (years)	16 [9-18]	12 [9-13]	15 [8-20]	0.470 ^c	
Premorbid IQ (WAIS-III Vocabulary)	45.4 (9.4)	43.9 (13.8)	49.3 (8.3)	0.325 ^a	
Disease duration (years)	7.47 (4)	6.65 (4.6)	-	0.583 ^d	
UPDRS-III	20.31 (9.6)	25.90 (7)	-	0.122 ^d	
H&Y stage	2 [1.5-2.5]	2 [1.5-3]	-	0.492 ^b	
LEDD _{DA}	395 [57.75-400]	300 [37.5-300]	-	0.838 ^e	
LEDD _{TOTAL}	1210 [613-1449]	725 [487-1131]	-	0.089 ^e	
PDQ-8	7.69 (4.9)	5.25 (2.9)	0.41 (0.9)	0.0001 ^a	PDICD>HC (p=0.0001) PDnoICD>HC (p=0.0001)
MoCA	27 (2.2)	27.3 (3)	28.3 (1.7)	0.444 ^a	
HADS total	8 [5-18.2]	4 [1.2-5.7]	5 [4-7]	0.015 ^c	PDICD>PDnoICD (p=0.007) PDICD>HC (p=0.048)
HADS-anxiety	4.5 (3.2)	3.65 (2.1)	4.47 (2.6)	0.166 ^a	
HADS-depression	3.5 [1-5.7]	1 [0-2.7]	1 [0-2.5]	0.003 ^c	PDICD>PDnoICD (p=0.003) PDICD>HC (p=0.004)
QUIP-RS score	16 (12.2-26.7)	-	-	-	
TCI-R Novelty Seeking total	99 [92.2-108.5]	85 [73-92.7]	91.7 [86.5-97]	0.009 ^c	PDICD>PDnoICD (p=0.002)
NS1 Exploratory excitability	29.2 (7.1)	25.1 (7)	27.7 (4)	0.148 ^a	
NS2 Impulsiveness	25.8 (6.6)	18.1 (6.5)	23.5 (5.3)	0.002 ^a	PDICD>PDnoICD (p=0.002)
NS3 Extravagance	26.9 (4.5)	22.9 (6.3)	25.9 (5.3)	0.085 ^a	
NS4 Disorderliness	18.3 (6.4)	14.5 (5.1)	16.6 (3.8)	0.033 ^a	PDICD>PDnoICD (p=0.032)
Barratt Impulsiveness total	40 [28.2-61.2]	29.5 [25.2-34.5]	33.5 [27.5-40.5]	0.020 ^a	PDICD>PDnoICD (p=0.020)
Barratt Attention	13.9 (6.7)	9.4 (4.4)	12.8 (4.5)	0.031 ^a	PDICD>PDnoICD (p=0.040)
Barratt Motor Impulsivity	15.3 (7.6)	10.1 (5)	13.4 (5)	0.024 ^a	PDICD>PDnoICD (p=0.037)
Barratt Non-planning	14.8 (8.6)	9.6 (3.8)	11.2 (5.7)	0.045 ^a	PDICD>PDnoICD (p=0.042)
Starkstein score	4.5 [1-14.7]	2.5 [1-6.7]	0 [0-3]	0.283 ^c	

Values expressed in mean (SD) in parametric variables, in median and IQ range in non-parametric variables

^a ANOVA

^b Chi-Square

^c Kruskal-Wallis

^d Two-sample T-test

^e U Mann Whitney

Abbreviations: IQ = Intelligence Quotient; WAIS-III = Wechsler Adult Intelligence Scale-III; UPDRS = Unified Parkinson's Disease Rating Scale; H&Y=Hoehn and Yahr scale; LEDD_{TOTAL}= Total daily levodopa equivalent dose. LEDD was calculated using the following formula $LED (mg) = (1 \times \text{levodopa}) + [0.77 \times \text{levodopa controlled release (CR)}] + (1.43 \times \text{levodopa} + \text{entacapone}) + (1.11 \times \text{levodopa CR} + \text{entacapone}) + (20 \times \text{ropinirole}) + (20 \times \text{ropinirole ER}) + (100 \times \text{pramipexole}) + (30 \times \text{rotigotine}) + (10 \times \text{bromocriptine}) + (8 \times \text{apomorphine}) + (100 \times \text{pergolide}) + (67 \times \text{cabergoline})$ (Parkin et al., 2002); LEDD_{DA}: daily levodopa equivalent dose of dopamine agonist according to the same formula; HADS=Hospital Anxiety and Depression Scale; ; QUIP-RS= Questionnaire for Impulsive-Compulsive Disorders in Parkinson's Disease-Rating Scale; TCI-R=Revised Temperament and Character Inventory; NS=Novelty Seeking Subscales.

Figure 1. The 40 independent components (ICs) identified by a group ICA. (A) Spatial maps of the 40 ICs divided into seven networks. (B) Connectogram representing the connections between the ICs. Yellow lines represent positive functional connectivity, and blue lines represent negative functional connectivity (C) Group averaged static functional connectivity between IC pairs was computed using the entire resting state data. The value in the correlation matrix represents the Fisher's z-transformed Pearson correlation coefficient. Each of the 40 IC was rearranged by network group based on the seven functional networks. Index numbers of independent components are written on the left and bottom side of the matrix. Correlations between the ICs are represented in a scale from red (higher) to blue (lower).

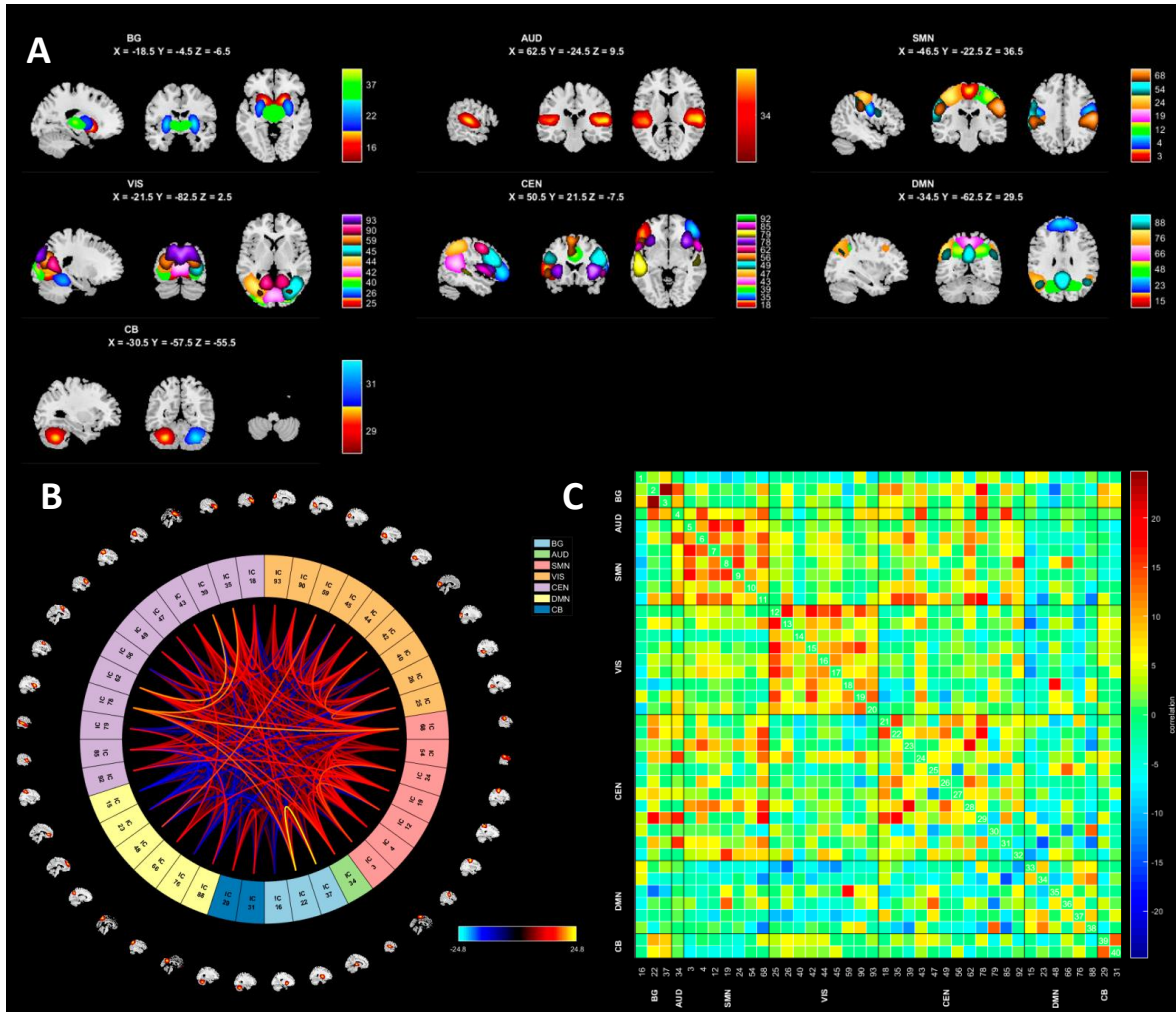


Figure 2. Dynamic FNC states resulting from the clustering analysis. A) Functional network connectivity matrices for each state, indicating the total occurrences and the percentages. Correlations between the ICs are represented in a scale from red (higher) to blue (lower). B) Connectogram representing the connections between the ICs (Yellow lines represent positive functional connectivity, and blue lines represent negative functional connectivity). C) Only that 5% of the functional connectivity matrix, representing the strongest connections (i.e. the largest absolute value correlation coefficients) is shown for each state. Red lines represent positive functional connectivity, and blue lines represent negative functional connectivity.

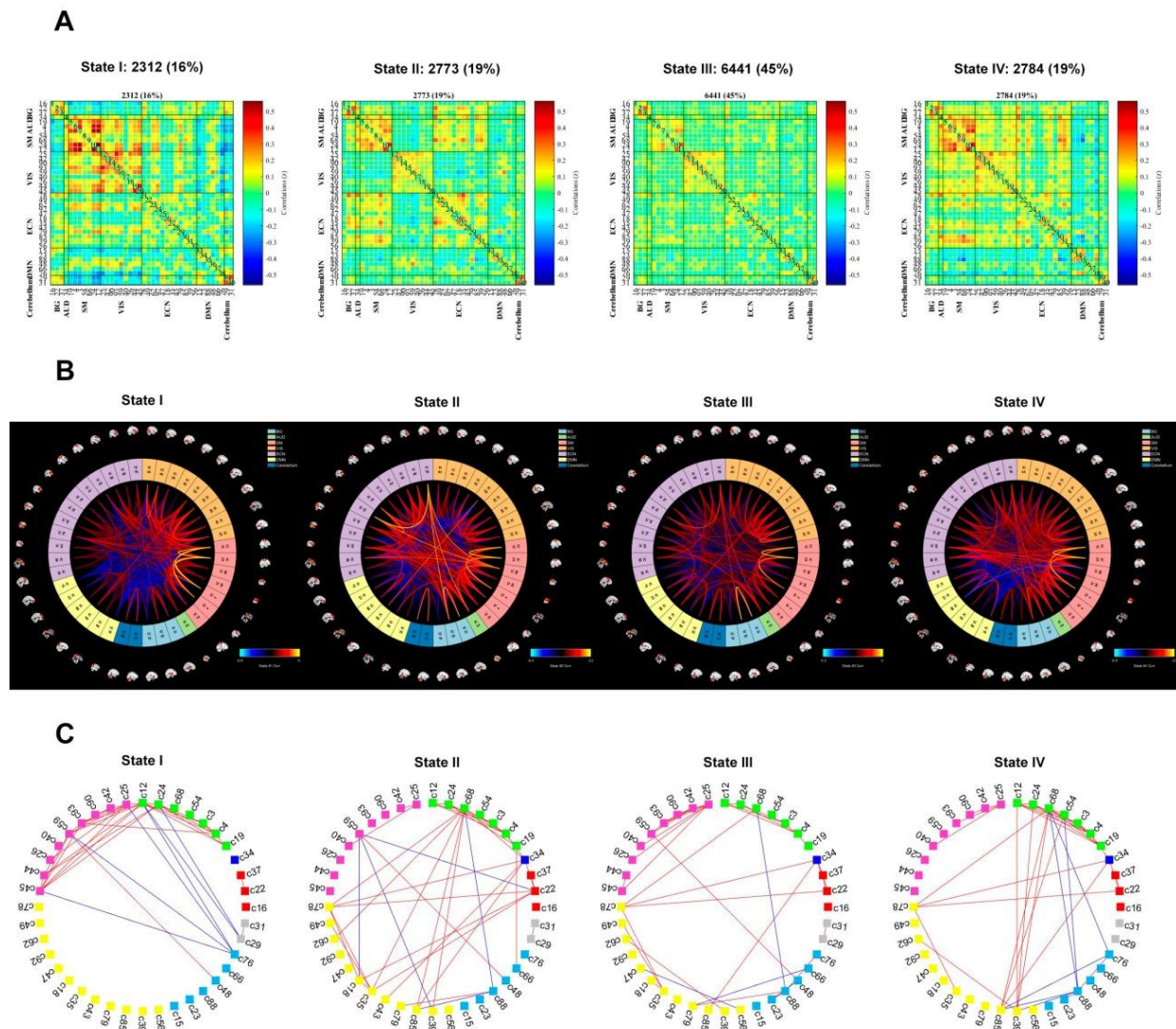


Figure 3: A) Differences in the temporal properties of the dynamic functional network connectivity states between the groups. (1) Mean dwell time (DT) between the groups and the significant differences between the groups in State III (&= PD-ICD>HC; \$=PD-ICD>PD-noICD) (2) Mean fractional window (FW) spent by the subjects in each state. B) Correlation of the clinical features of the PD-ICD group with the temporal properties detected. (1) The mean dwell time (DW) of State III was positively correlated with the NS sub-scale of the TCI-R scale (Novelty Seeking) and with the non-planning sub-scale of the BIS scale (Barratt Impulsiveness scale). (2) The fractional window (FW) of State III was positively correlated with the non-planning sub-scale and with the total BIS score.

