

Cholesterol constrains the antigenic configuration of the membrane-proximal neutralizing HIV-1 epitope

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3 The envelope glycoprotein (Env) enables HIV-1 cell entry through fusion of host-cell
4 and viral membranes induced by the transmembrane subunit gp41. Antibodies targeting
5 the C-terminal sequence of the Membrane-Proximal External Region (C-MPER) block
6 the fusogenic activity of gp41 and achieve neutralization of divergent HIV-1 strains and
7 isolates. Thus, recreating the structure that generates broadly neutralizing C-MPER
8 antibodies during infection is a major goal in HIV vaccine development. Here, we have
9 reconstituted a peptide termed CpreTM-TMD in a membrane environment. This peptide
10 contains the C-MPER epitope and the minimum TMD residues required for the
11 anchorage of the Env glycoprotein to the viral membrane. In addition, we have used
12 antibody 10E8 variants to gauge the antigenic configuration attained by CpreTM-TMD
13 as a function of the membrane cholesterol content, a functional determinant of the HIV
14 envelope and liposome-based vaccines. Differential binding of the 10E8 variants and the
15 trend of the IgG responses recovered from rabbits immunized with liposome-peptide
16 formulations, suggested that cholesterol may restrict 10E8 accessibility to the C-MPER
17 epitope. Our data ruled out the destabilization of the lipid bilayer architecture in
18 CpreTM-TMD-containing membranes, and pointed to the perturbation of the helical
19 conformation by lipid packing as the cause of the antigenic configuration loss induced by
20 cholesterol. Overall, our results provide additional insights into the structural basis of the
21 Env complex anchoring to membranes, and suggest new approaches to the design of
22 effective immunogens directed against the near pan-neutralizing HIV-1 epitope C-
23 MPER.
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52 Keywords: HIV-1 MPER; HIV-1 TMD; neutralizing antibody 10E8; MPER vaccine; membrane
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3 Fusion with the target host-cell membrane marks the beginning of the Human
4 Immunodeficiency Virus type-1 (HIV-1) replication cycle ¹⁻⁴. The transmembrane
5 subunit gp41 of the envelope glycoprotein (Env) promotes the process by the concerted
6 action of two types of structural elements: i) two highly conserved membrane-inserting
7 regions, one at the free N-terminus and the other proximal to the viral membrane ⁵; and
8 ii) helical domains or heptad repeats (HRs) that refold forming an energetically
9 favorable, trimeric 6-helix bundle ⁶. The membrane-inserting sequence at the N-
10 terminus constitutes the fusion peptide (FP) (reviewed in ⁵). After fusion triggering by
11 receptor (CD4)/co-receptor engagement (CXCR4 or CCR5), the FP is propelled towards
12 the cell membrane and embeds therein due to its hydrophobic character ²⁻⁴. However, the
13 tip of the FP remains exposed to the solvent in one of the conformational states of the
14 pre-fusion Env complex ⁷⁻⁸, and is accessible to antibodies that neutralize HIV-1 with
15 modest potency and breadth ⁹⁻¹⁰.

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34 The sequence inserting into the viral membrane, also known as the Membrane-Proximal
35 External Region (MPER), is exceptionally enriched in aromatic residues that promote
36 interactions with the membrane interface ¹¹⁻¹⁴. Structural analyses suggest that the C-
37 terminal residues of MPER (C-MPER, Env residues 671-683, HXB2 numbering) can
38 combine with N-terminal residues of the transmembrane domain (TMD, Env residues
39 684-690) into a single continuous helix ¹⁵⁻²¹. CpreTM, a peptide spanning this region
40 can induce lipid bilayer restructuring upon partitioning into cholesterol (Chol)-enriched
41 virus-like membranes ²²⁻²⁴. Thus, the membrane activity of this sequence, unleashed
42 after fusion activation, is postulated to help the fusion process proceed by perturbing the
43 highly rigid HIV lipid envelope ²⁵ (Fig S1a).

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58 Importantly, the conserved C-MPER sequence is immunogenic during infection ²⁶⁻²⁸,
59 which underscores the existence of a structurally stable state of this Env region
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3 accessible to B-cell receptors, at least within one of the conformational states visited by
4 the pre-fusion complex ²⁹⁻³⁰. Further supporting the existence of a structurally defined
5 C-MPER epitope common to diverse pre-fusion Env variants, all anti-C-MPER broadly
6 neutralizing antibodies (bnAbs) that have been isolated so far (e.g, 4E10, 10E8 or
7 LN01), recognize the same surface of the C-MPER helix, and consistently display the
8 broadest coverage among the HIV-1 bnAb classes ^{21, 26-27, 31-34}. Using super-resolution
9 microscopy we have recently demonstrated that C-MPER is indeed accessible to the
10 bnAbs 4E10 and 10E8 on the surface of intact virions ³⁵.

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12 Atomic structure resolution of bnAbs 4E10, 10E8 and LN01 in complex with lipids ^{21,}
13 ³⁶⁻³⁷, or with epitope-peptides elongated to include TMD residues ^{19, 21}, in combination
14 with cryo-electron microscopy (cryo-EM) reconstructions of Env-Fab complexes ^{17, 34},
15 has provided a model for the molecular recognition of C-MPER at the virus membrane
16 surface (Figure 1). According to this model, monomers of continuous helices spanning
17 the MPER-TMD region stick out the membrane with similar topologies, with angles
18 ranging from slightly tilted to almost perpendicular to the membrane plane, and
19 antibodies nonspecifically adsorbed to the interfacial region of the membrane approach
20 the C-MPER epitope laterally. However, in analogy with the dynamic conformation of
21 the pre-fusion Env ectodomain ^{7-8, 29-30}, cumulative evidence supports the
22 conformational pliability of MPER-TMD helices, which, depending on the sequence
23 range considered, membrane dose and lipid composition, may adopt in the unbound
24 conformation membrane structures differing in oligomeric state, insertion angle or C-
25 MPER epitope exposure ^{13-15, 18, 20, 38-39}. Interestingly, recent studies report a
26 transmembrane helix tilt angle of ca. 45° for a TMD peptide elongated at its C-terminus
27 ²⁰ or the total occlusion of C-MPER antigenic face into the membrane when a peptide is
28 elongated to contain the full MPER sequence at its N-terminus ¹³. Thus, the membrane-

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3 inserted states adopted by these peptides appear to be incompatible with the proposed
4 mechanism of lateral Env docking of anti-C-MPER antibodies ^{17, 19, 36-37}.
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8 In an attempt to mimic the membrane-inserted MPER structure that elicits anti-C-
9 MPER antibodies, in this study we have addressed the reconstitution of the C-MPER
10 epitope recognized by bnAb 10E8 in liposome vaccines. To that end, we employ
11 peptides that combine the C-MPER epitope with the minimal TMD anchor of Env
12 previously described by Yue et al. ⁴⁰ In addition, we have generated bnAb 10E8 mutants
13 that can be used as reference standards to measure the antigenicity profile of the
14 reconstituted peptides. We demonstrate that the C-MPER epitope can attain a correct
15 configuration in membranes, but that high concentration of Chol induces its
16 concealment. We propose a model that, besides providing new insights into the
17 molecular basis of Env-anchoring to the viral membrane, may inform the design of
18 immunogenic formulations aimed at boosting anti-C-MPER bnAb production.
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RESULTS

Design of a C-MPER epitope peptide with a membrane anchor

The model in Figure 1a reflects the capacity of the native Env trimer for sampling different conformational states³⁰, with the C-MPER epitope becoming accessible to the bnAb 10E8 within one of such states³⁵. Panel 1b displays a detailed view of 10E8 docking to Env in the pre-fusion state^{17, 19, 37}. From this model one can infer that 10E8 binding to Env would freeze the CpreTM region in an upright position, preventing further interaction with the viral membrane and, hence, fusion to proceed (Figure S1a). Panel 1b highlights the three elements of the Fab 10E8 involved in the efficient engagement with the C-MPER epitope at membranes, namely, (1) the specificity binding pocket, (2) an accommodation surface with the membrane interface, and (3) an area in contact with the Env complex ectodomain^{19, 26, 37}.

As explained in the diagrams depicted in Figures 1c and S1b, in this study we seek to reproduce the components (1) and (2) of the interaction by reconstituting in liposome vaccines the peptide CpreTM-TMD (Env residues 671-700, HXB2 numbering). This peptide encompasses the full 10E8 epitope and a minimal membrane anchor of Env⁴⁰. In addition, it contains Lys-tags to increase solubility at both ends of the molecule¹⁶. In contrast to the shorter CpreTM peptide that destabilizes the membrane architecture^{22, 24-25}, or longer peptides that seem to conceal the C-MPER epitope^{13, 20, 38}, we expected the CpreTM-TMD peptide to span the lipid bilayer without affecting its integrity, and to expose the antigenic face of the C-MPER helix accessible for its engagement with antibodies and B-cell receptors (Figure 1c, right). Thus, in our approach we reasoned that a scaffold peptide with a minimal TMD would force the upright orientation of the

helix and ensure at the same time an efficient exposure of the C-MPER epitope at the membrane interface (Figure S1b).

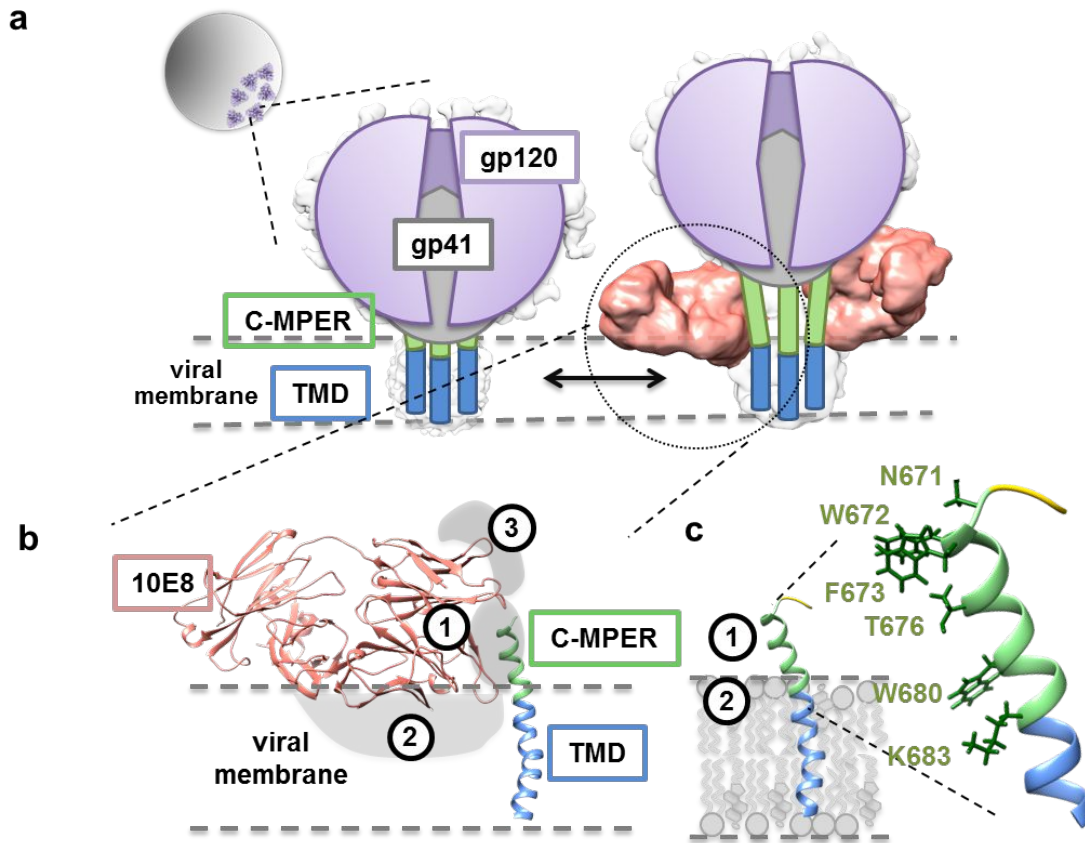


Figure 1: Schematics depicting the accessibility of the HIV-1 neutralizing epitope MPER at the viral membrane interface. (a) Model for accessibility of the C-terminal section of MPER (C-MPER) based on cryo-EM reconstructions of native Env complexes¹⁷. Back contours are derived from detergent-solubilized Env trimers, without (right, EMDB-3308) or with 10E8 bound (left, EMDB-3312). Transition between both states would result in accessibility to MPER helix in native Env (green). **(b)** Structural model for 10E8 recognition of the helical C-MPER epitope inserted in membranes. The position of the TMD residues (blue) was rendered by superimposing residues N671-V689 of MPER in complex with Fab 10E8 (PDB ID: 5GHW) onto structures of MPER-TMD peptides (PDB ID: 2MG1, 2MG2). Numbers denote the interaction-accommodation surfaces in the Fab after binding to C-MPER epitope (see main text). **(c)** Schematics of the liposome-peptide vaccines used in this study, which contain the reconstituted CpreTM-TMD peptide (in ribbon representation, lysine tag depicted in yellow). Left panel: numbers denote the attempt to recover through vaccination antibodies that bind to C-MPER epitope (1); and develop a surface to accommodate the membrane interface (2). Right panel: antigenic face of the C-MPER helix. Main epitope residues that interact with the 10E8 paratope are depicted in stick representation.

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3 **Functional characterization of bnAb 10E8 variants used to assess C-MPER**
4 **exposure.**
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8 Fab 10E8 binding to membranes containing CpreTM-TMD reflects the accessibility to
9 the C-MPER epitope at the membrane surface. As explained above, Fab binding implies
10 not only the adequate fitting of the specificity pocket of the antibody to its MPER
11 epitope, but also the correct positioning of the antibody at the membrane interface.
12 Thus, in our approach we assumed that alteration of the Fab surface that accommodates
13 the membrane interface might promote or diminish the capacity of 10E8 to bind its
14 epitope. Following this rationale we generated two Fab 10E8 variants that, along with
15 the WT Fab, were used as standard references to gauge the correct membrane topology
16 of the C-MPER epitope (Figure 2a). The LC.S65W mutation added a Trp at the Fab
17 surface that accommodates the viral membrane, and was expected to enhance the
18 binding of the Fab to Env by increasing its affinity for the membrane interface ^{35, 41}.
19 Conversely, the HC.W100bD mutation was designed to interfere with the membrane
20 insertion of the heavy chain complementarity-determining region 3 loop (HCDR3) of
21 the Fab ^{19, 42}.
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41 Super-resolution fluorescence microscopy experiments confirmed the differential
42 binding of the 10E8-based Fabs to native Env on intact virions ³⁵. Quantitative
43 stimulated emission depletion (STED) microscopy offers a spatial resolution of < 40
44 nm, below the size of HIV virions (around 125 nm), which allowed us to unequivocally
45 identify the antibody signal coming from viral particles and resolve features within
46 them ⁴³. Moreover, due to the linear nature of STED microscopy, the number of photons
47 recorded is directly proportional to the amount of fluorescent molecules, which
48 permitted quantification of antibody binding ³⁵. Figure 2b displays microscopy images
49 of individual Vpr.EGFP-labeled viral particles incubated with Fab 10E8 WT or its
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variants, LC.S65W and HC.W100bD (left panels), whose binding to Env on the particles was visualized by directly labeling Fabs with the STED-able Aberior STAR RED (also known as KK114) dye and also using a STAR RED-labeled secondary antibody.

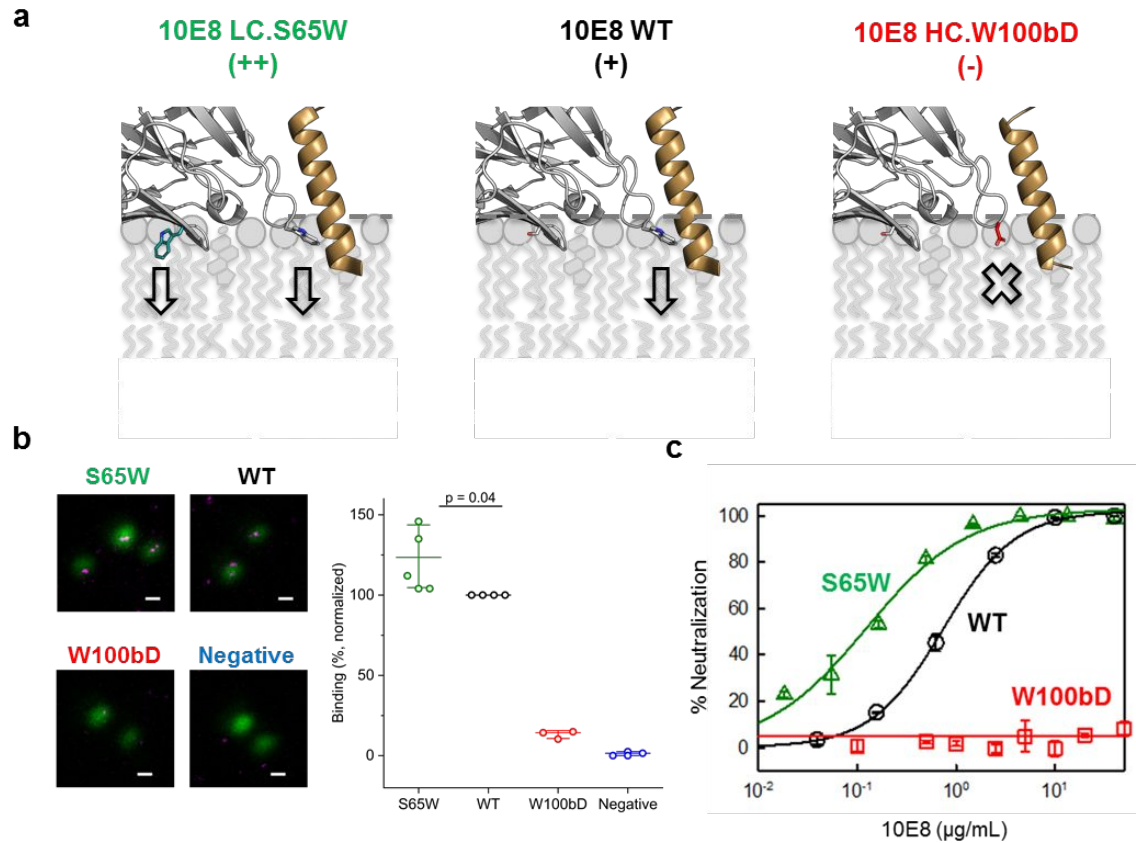


Figure 2: Functional properties of Fab 10E8 variants. (a) Structural model of gp41 C-MPER at the membrane interface in complex with Fab 10E8 WT (PDB ID: 5GHW, middle panel). LC.S65W and HC.W100bD variants are depicted in left and right panels, respectively. HC.W100b residue and mutated residues LC.S65W and HC.W100bD are displayed in stick representation. Arrows indicate the potential capacity of each Fab to anchor to the membrane. (b) Binding of Fab 10E8 WT and its mutants to native Env, measured by quantitative STED microscopy. Left: micrographs of HIV virions (EGFP.Vpr confocal signal, green) and 10E8 variants (STAR RED, magenta). Scale bar is 200 nm. Right: STED intensity signals (sum of collected photons) detected on single virions for each antibody were normalized to the signal of Fab WT after background subtraction. Each point is an independent experiment, middle horizontal bar represents the median and whiskers the SD. The number of individual virions analyzed in every experiment was at least 150 and typically around 400 for every condition (See Supplementary Figure S2 for single virus data). Negative corresponds to viruses untreated with Fabs. (c) Neutralization potency of 10E8 Fab variants. Dose-response curves follow cell entry inhibition measured against HIV-1 virions pseudotyped with JR-CSF Env. Data for WT, LC.S65W and HC.W100bD are shown with circles (black), triangles (green) and squares (red), respectively, and correspond to mean values (\pm SD) from two replicate wells in a representative experiment.

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3 As hypothesized, quantitative analysis of the antibody signal in individual virions
4 followed the trend: 10E8-LC.S65W > 10E8-WT > 10E8-HC.W100bD, with an average
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8 24% increased binding of the LC.S65W variant to Env as compared to the WT version,
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10 and an 87% binding decrease of the HC.W100bD mutant (Figure 2b right panels and
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12 Figure S2). The capacity of these Fab 10E8 variants to bind to MPER on intact virions
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14 further correlated with their neutralization potency (Figure 2c). Therefore, we conclude
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16 that this binding pattern has to be reproduced by any relevant peptide epitope proposed
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18 as a vaccine candidate targeting 10E8-like antibody responses.
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26 **C-MPER accessibility in liposome vaccines containing reconstituted CpreTM-**
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31 Chol acts as modulator of the structure-function of integral membrane proteins, thereby
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33 affecting the exposure of cell surface/membrane anchored therapeutic targets such as
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35 GPCRs, ion channels, transporters, or growth factor receptors⁴⁴⁻⁴⁵. Folding of the gp41
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37 MPER-TMD region also takes place in the Chol-enriched environment of the viral
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39 membrane⁴⁶⁻⁴⁷, hence, this compound is assumed to play a role in C-MPER
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41 immunogenicity and its molecular recognition by 10E8. Furthermore, the stability and
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43 immunogenicity of liposome-based vaccine formulations are customarily enhanced by
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45 inclusion of Chol in the lipid composition¹⁴. Using the Fab 10E8 variants described in
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47 the previous section, we next determined the exposure of the C-MPER epitope in
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49 liposome-peptide formulations (LPFs) proposed as vaccines, which consisted of the
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51 CpreTM-TMD peptide reconstituted into liposomes composed of POPC:PA and 0, 20,
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53 40 or 50 % Chol (Figure 3). LPFs were generated by mixing the CpreTM-TMD peptide
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55 with POPC:PA:Chol lipids in organic phase prior to generation of the liposome
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particles. Sucrose density gradient ultracentrifugation proved full incorporation of CpreTM-TMD to membranes after the reconstitution procedure (Figures S3). Moreover, the resulting LPFs did not differ significantly in size (Figure S4).

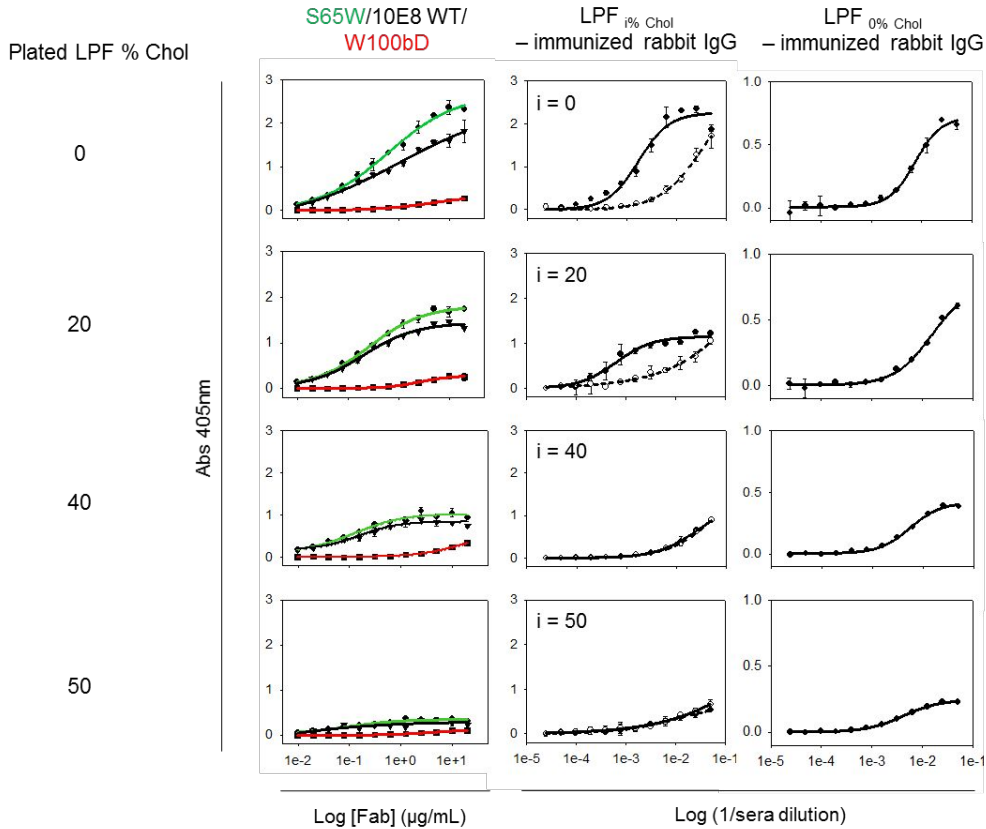


Figure 3. Antigenic profile and immunogenicity of liposome-peptide formulations. ELISAs were performed with liposome-peptide formulations (LPFs) containing CpreTM-TMD (peptide-to-lipid mole ratio, 1:50) that were coated on plates at a concentration of 500 μ M and containing increasing concentrations of Chol as indicated in the panels. Plotted absorbance values are means (\pm SD) from two replicate wells. Left panels: comparative binding of Fab 10E8 variants WT (black line and filled triangles), LC.S65W (green line and filled circles) and HC.W100bD (red line and filled squares). Middle panels: immunogenicity of LPFs, as measured by the presence of IgG antibodies in the sera of two different rabbits after immunization. Signal of the pre-immune sera was subtracted. Right panels: cross-reactivity of IgG produced in sera of rabbits immunized with LPFs devoid of cholesterol, against LPFs with increasing cholesterol concentration. Sera from the two animals were pooled and the IgG levels in the mixture subsequently detected by ELISA. In all cases, experimental values were adjusted to sigmoid dose-response curves.

Binding of Fab 10E8 variants to LPFs coated on ELISA plates followed in all instances the expected trend for a correctly exposed epitope: 10E8-LC.S65W > 10E8-WT > 10E8-HC.W100bD, but the binding levels decreased greatly in samples containing the

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3 highest Chol concentrations (Figure 3, left panels). Thus, high doses of Chol seemed to
4 conceal the 10E8 epitope of the reconstituted CpreTM-TMD peptide. Similar results
5 were obtained for KK114-labeled 10E8 variants interacting with CpreTM-TMD peptide
6 reconstituted in Giant Unilamellar Vesicles (GUVs) made of the same lipid mixtures
7 (Figure S5).
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15 A similar trend was observed for the serum IgG produced after immunization of rabbits
16 with the LPF vaccines. Thus, the amount of IgG that bound to LPF immunogens also
17 decreased with the content of Chol present in the formulations (Figure 3, center panels).
18 Interestingly, IgG produced in rabbits immunized with the LPF devoid of Chol, also
19 trended to lower binding to the LPFs containing increasing concentrations of Chol
20 (Figure 3, right panels). Thus, Chol may have restricted the accessibility of B-cell
21 receptors to C-MPER, and also that of the IgGs produced upon immunization with LPFs
22 bearing an accessible C-MPER epitope.
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33 34 35 36 37 **Stability of liposome vaccines with reconstituted CpreTM-TMD**

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40 Membrane-active peptides can generate fusion-related perturbations in lipid bilayers ⁵.
41 We have previously reported that pre-loading Chol-enriched vesicles with CpreTM
42 rendered them competent for subsequent lipid-mixing with target vesicles ^{23, 25}.
43 Therefore, CpreTM can alter the membrane integrity of Chol-enriched membranes to
44 make them competent for fusion. Since vesicle fusion with cellular membranes might
45 diminish the fraction of C-MPER epitope accessible for engagement with the
46 components of the immune system, we next analyzed whether CpreTM-TMD-
47 containing liposome vaccines were also inherently unstable and prone to fusion (Figure
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3 To test this, we used a heterotypic fusion assay, in which GUVs that mimicked the
4 composition and curvature of the cell plasma membrane external leaflet were the targets
5 for LPFs primed for fusion by incubation with C-MPER containing peptides. Incubation
6 of GUVs with CpreTM-primed LPFs led to the homogeneous labeling of the GUV
7 membranes with the fluorescent LPF label, indicative of LPFs mixing their membrane
8 lipids with those of GUVs. Consistent with previously published bulk measurements ²³,
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10 ²⁵, this effect was only observed when CpreTM was administered together with vesicles
11 containing high concentrations of Chol. Conversely, incubation of fluorescently-labeled
12 CpreTM-TMD liposome vaccines with target GUVs did not lead to dye transfer under
13 any condition, demonstrating that CpreTM-TMD-containing LPFs are not prone to
14 fusion, not even when they contain a high proportion of Chol.
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29 To inquire whether the non-fusogenic CpreTM-TMD peptide reconstituted in Chol-
30 containing membranes could still perturb locally the integrity of the lipid bilayer, we
31 next determined the permeability of the membranes composing the different LPF
32 vaccines also using a single-vesicle approach ⁴⁸. Confocal micrographs of GUVs
33 matching the lipid composition of the LPFs, and containing CpreTM-TMD are depicted
34 in Figure 4b. In addition, vesicles lacking peptide or vesicles treated with the peptide
35 CpreTM were used as a control for negative permeabilization or effective
36 permeabilization, respectively ²², ⁴⁸. Both untreated and CpreTM-TMD-containing
37 GUVs were viewed as dark (empty) spheres surrounded by the NBD-labeled lipid
38 bilayer (depicted in green color), against a background containing the permeant KK114
39 fluorescent probe, (rendered in red color). In contrast, incubation with the CpreTM
40 peptide resulted in the red labeling of the internal compartments, consistent with the
41 permeabilization of the lipid bilayer to the dye in the external solution ⁴⁸.
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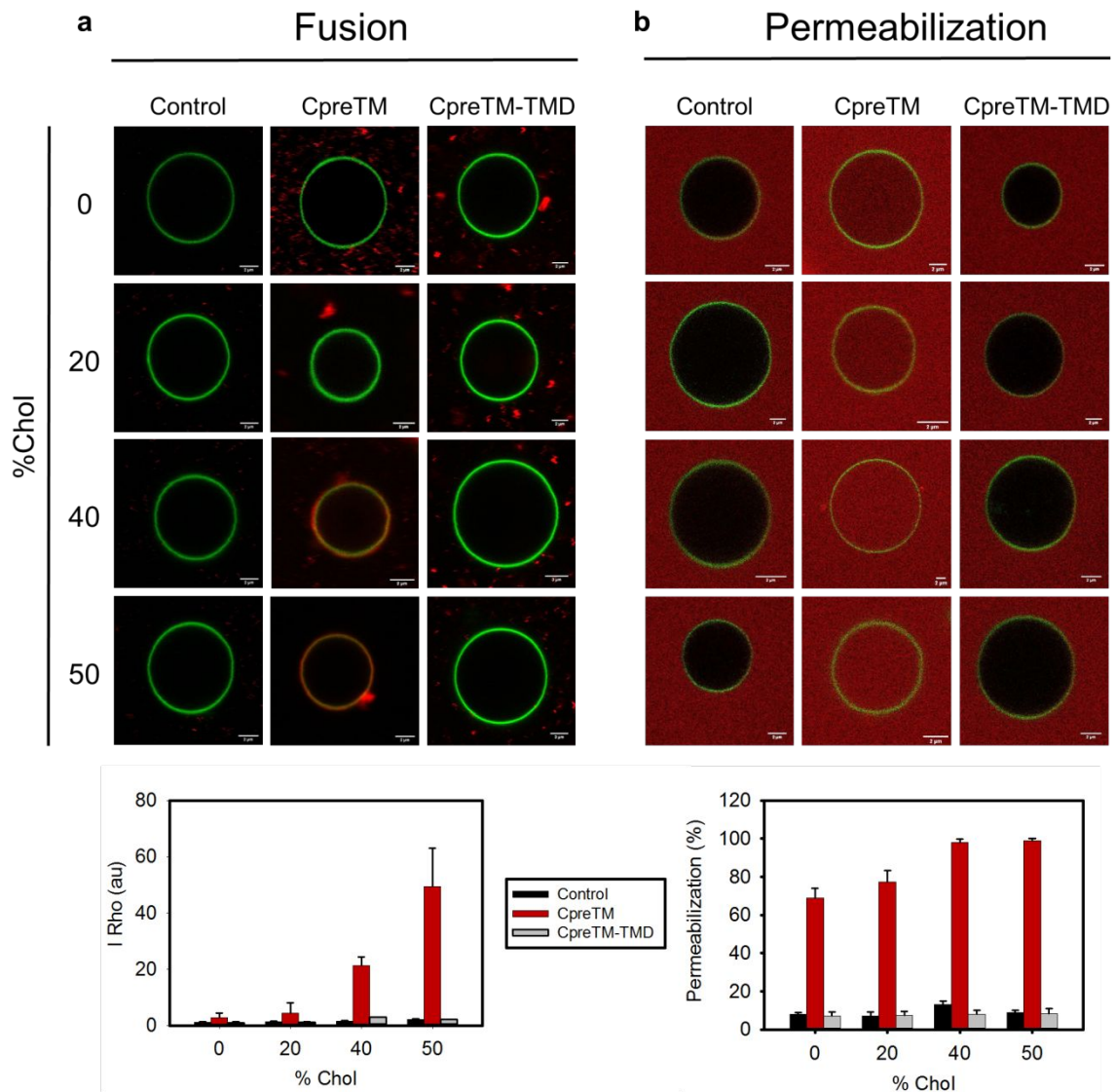


Figure 4: Stability of CpreTM-TMD-containing lipid bilayers measured in single-vesicle assays. (a) Channel-merged confocal fluorescence microscopy images of a heterotypic fusion assay between NBD-labeled GUVs mimicking the outer leaflet of cell plasma membrane (green) and Rho-labeled LUVs of varying cholesterol concentrations (red) in the absence (control) or presence of CpreTM or CpreTM-TMD peptides (1:50 peptide-to-lipid mole ratio). Rhodamine dye transfer to GUV membranes is indicative of lipid-mixing. The bottom plot shows the relative extents of fusion obtained by measuring the fluorescence intensity of the Rho dye at the membrane of each GUV after co-incubation with LUVs for 60 min (mean fluorescence values \pm SD of 5 different vesicles per composition). (b) Channel-merged micrographs of single GUV permeabilization assays. NBD-labeled GUVs matching the lipid composition of the LUVs (green circumferences) and containing CpreTM, CpreTM-TMD or no peptide, were immersed in a solution containing the water soluble KK114 fluorescent probe (red background). The presence of KK114 inside the vesicles indicates effective permeabilization. The bottom plot shows relative permeabilization levels after 60 min incubation (mean fluorescence values \pm SD of 5 different vesicles per composition).

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3 Even though the absence of bilayer perturbations in samples that contained CpreTM-
4 TMD was apparent after microscopic examination, we also performed quantitative
5 measurements of fluorescence in selected GUVs (lower panels of Figure 4). These data
6 further illustrate the absence of peptide-induced effects (i.e., ground-like levels of Rho
7 or KK114 fluorescence in membrane or lumen, respectively).
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18 **Lipid packing changes and peptide conformational transitions in LPFs**

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21 Overall, the previous results demonstrate that the reconstituted CpreTM-TMD peptide is
22 devoid of the membrane activity of the CpreTM section, suggesting that membrane
23 restructuring is not the cause of the C-MPER epitope concealment observed in Chol-
24 rich LPFs. Chol also induces a dose-dependent lipid packing increase when
25 incorporated into lipid bilayers⁴⁹. It has been suggested that the “cholesterol
26 recognition/interaction amino acid consensus” motif^{679LWYIK/R683} present in
27 CpreTM-TMD could sequester Chol^{24, 50}, and interfere with lipid packing, making
28 bilayers more fluid, a biophysical effect that may condition immunogenicity of the
29 LPFs¹⁴. Thus, we next performed two-photon fluorescence imaging of Laurdan-stained
30 GUVs to quantitatively determine lipid packing in the liposome-based vaccines that
31 contained different amounts of Chol^{24, 47}. The emission spectrum of Laurdan changes in
32 response to polarity. In a membrane context, changes in polarity are ascribed to
33 differences in lipid packing, which influences water accessibility. The Generalized
34 Polarization (GP) ratiometric parameter quantifies Laurdan’s emission spectral shift
35 from tightly packed bilayers (high GP value) to loosely packed membranes (low GP
36 value), thus providing an *in situ* estimation of membrane packing.
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3 Figure 5a displays GP images of POPC:PA GUVs containing increasing Chol
4 concentrations. The bottom panels include vesicles that incorporated the
5 reconstituted CpreTM-TMD peptide. Mean average GP values increased with Chol
6 concentration in the samples, as expected from the ordering effect exerted by this
7 compound in lipid bilayers. Besides, the measured GP values demonstrated that
8 incorporation of the peptide had little effect on membrane order levels, ruling out
9 that the reconstitution process and/or potential specific interactions with Chol could
10 affect lipid packing in LPFs.
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22 It has been additionally argued that lipid packing augmented by Chol can affect
23 the accommodation of the transmembrane helices^{49, 51}. Thus, we next established
24 the influence of Chol on the conformation adopted by CpreTM-TMD in LPF
25 vaccines (Figure 5b). Infrared spectra in the amide-I region of CpreTM-TMD
26 reconstituted in POPC:PA LPFs exhibited absorption centered at 1654 cm⁻¹,
27 indicative of a main α -helical conformation adopted by the peptide⁵². Appearance
28 of a shoulder could be discerned in LPF samples that contained increasing
29 amounts of Chol, which was evidenced as a band centered at ca. 1620 cm⁻¹ at
30 the highest concentration of the compound. The growth of this band component
31 reflected accumulation of extended chains, a product of peptide partial unfolding.
32 Spectral changes could also be observed within the 1670-1660 cm⁻¹ range, ascribed to
33 absorption by conformers rich in 3_{10} -helix and turns. A relative contribution of the
34 different conformations to the overall CpreTM-TMD structure in membranes was
35 obtained after band decomposition of the LPF spectra (Figure S6).
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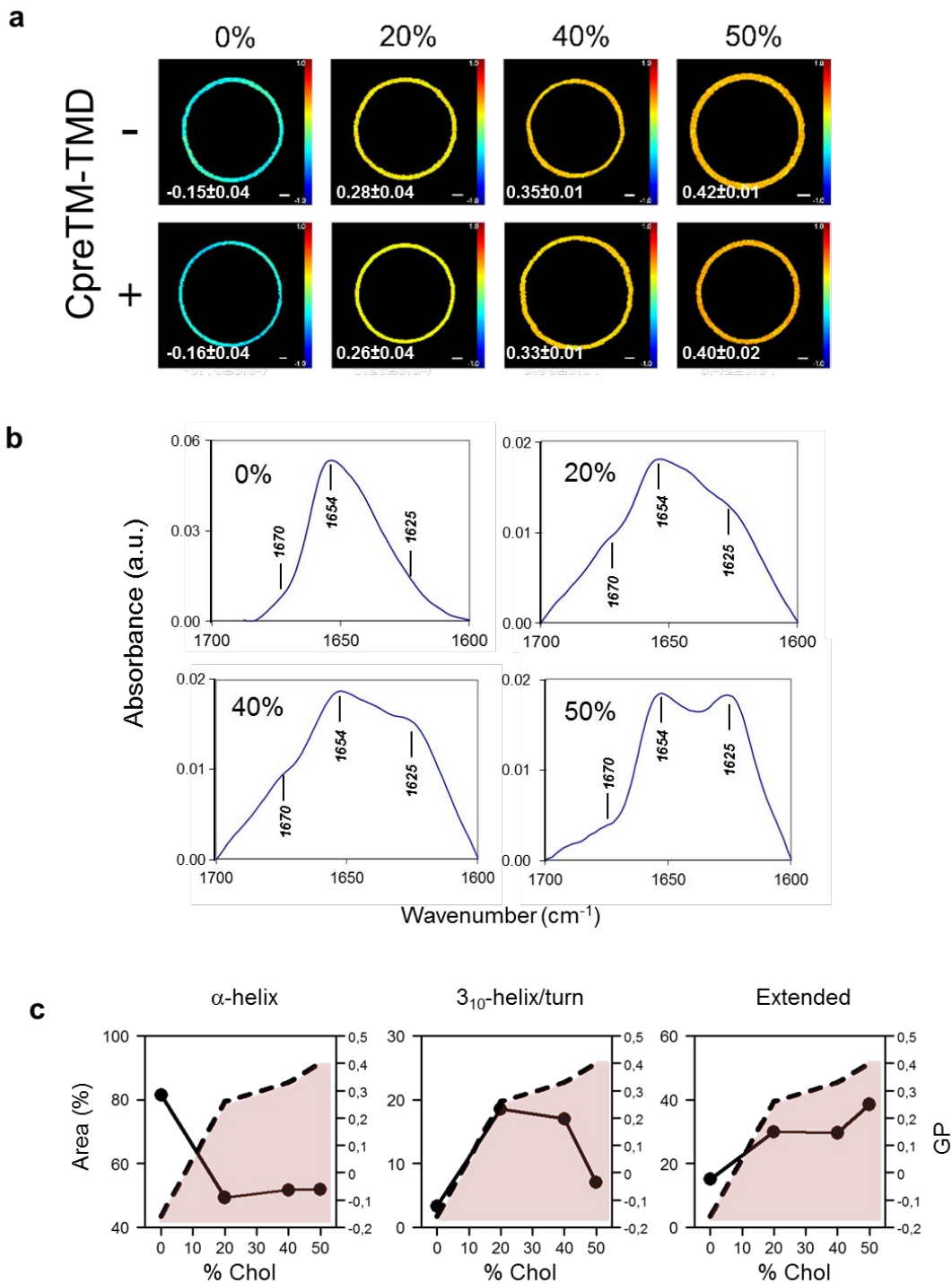


Figure 5: Lipid packing and structure of CpreTM-TMD in liposome-based formulations. (a) Laurdan GP images of single GUVs containing increasing cholesterol concentrations (0, 20, 40 or 50 mol %) with reconstituted CpreTM-TMD or in the absence of the peptide. High GP values (red) correspond to high molecular packing as opposed to lower GP values (blue) corresponding to more loosely packed membranes. Mean GP values \pm SD of more than 30 GUVs of two independent experiments are shown in the panels. Scale bar is 1 μ m. (b) IR spectra in the amide-I region of CpreTM-TMD reconstituted in LPFs containing increasing Chol concentrations. (c) Correlation between changes in CpreTM-TMD conformation (%Area), and lipid packing degree (Laurdan GP values). Contribution of the secondary structure components was calculated after IR amide-I band decomposition (Figure S6).

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Figure 5c illustrates the evolution of the different structural components (percentage of amide-I band area) as a function of the Chol content and lipid packing (GP value). The data suggest that an initial sharp increase in lipid packing correlates with a reduction of the α -helix content and an increment in the contribution of 3_{10} -helix and turns, consistent with the partial destabilization of the main helical conformation in the samples. Further addition of Chol resulted in accumulation of extended structures and reduction of 3_{10} -helix and turns. Together, the IR results suggest that Chol can alter gradually the conformation of the CpreTM-TMD helix inducing its partial unfolding.

Model for Chol-induced C-MPER epitope disruption

It has been recently described that TMDs with smaller solvent accessible surface areas accommodate more efficiently in highly packed membranes than those rich in bulkier residues.⁵¹ Consequently, most of the TMD helices found to reach the plasma membrane in eukaryote cells tend to segregate amino acids asymmetrically in two regions⁵³: residues containing short and less bulky side chains locate in the section that passes through the highly packed exoplasmic leaflet, whereas those with the more voluminous side chains, tend to remain in contact with the internal monolayer, where the disorder of the acyl chains is higher. This trend is reflected by the $\text{Surface Area}_{\text{exoplasmic}}/\text{Surface Area}_{\text{endoplasmic}}$ parameter, which measures the ratio of exoplasmic to cytoplasmic lipid-accessible surface areas of the helix⁵³. The value of this parameter is significantly less than 1 in the TMDs anchored to the plasma membrane.

Remarkably, as shown in Figure 6a, the Surface Area_{exoplasmic}/Surface Area_{endoplasmic} parameter calculated for the helix spanning the CpreTM-TMD region of HIV-1 is ca. 1.6, i.e., significantly higher than 1. Therefore, the CpreTM-TMD section rich in bulky residues is more prone to unfold in tightly packed lipid bilayers than the rest of the TMD region due to its comparatively larger surface area. We surmise that the increase in lipid packing causes the conformational changes of the MPER-TMD helix that result in the disruption of the C-MPER epitope (Figure 6b).

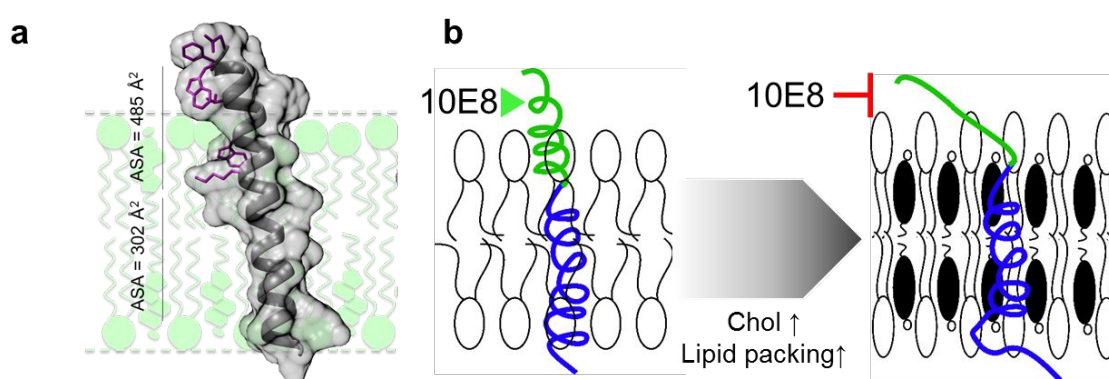


Figure 6: Model for restricted accessibility to C-MPER epitope in Chol-enriched membranes. (a) Asymmetry of CpreTM-TMD transmembrane helix surface area between halves of the lipid bilayer. Accessible surface areas were calculated as described^{51, 54}. (b) Cartoon illustrating unfolding of the CpreTM-TMD helix section containing the C-MPER epitope upon lipid-packing increase. Note that the model does not exclude chain extension also occurring at the C-terminal side of the helix, as previously proposed¹³.

DISCUSSION

The relevance of the C-MPER epitope as a target for vaccine design is highlighted by the discovery that broad and potent HIV-1 neutralizing activity of sera collected from chronically infected individuals can be in part mapped to this subregion^{26, 55-61}. Despite the interest in developing effective immunogenic formulations, as a general rule, vaccines against this site, are poorly immunogenic¹⁴. The available structural information on the mechanism of HIV bnAb binding to native C-MPER, suggests that

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3 an effective vaccine should elicit antibodies that i) engage with the integral membrane
4 antigen Env, ii) develop the ability to recognize specifically residues exposed on the
5 accessible face of the C-MPER helix, and iii) develop a surface to accommodate the
6 viral membrane interface (Figure 1).
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13 To formulate properly the C-MPER sequence at membrane surfaces, in this work we
14 have followed a new strategy (Figure S1). First, to focus immune responses to a single
15 epitope, the selected CpreTM-TMD peptide contains only the C-terminal subdomain of
16 MPER, which is followed by a minimal Env TMD that can effectively anchor the
17 protein in the membrane⁴⁰. We note that peptides containing the full MPER sequence
18 appear to occlude the C-MPER sequence in the membrane interface^{13, 62}, and tend to
19 raise responses focused on the N-terminal subdomain when formulated as LPFs (i.e.,
20 produce antibodies against the 2F5 epitope, but not against the 10E8 epitope)⁶².
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32 Second, we have generated functional variants of 10E8 and used them to gauge the
33 correct presentation of 10E8 epitope in LPFs. Our data indicate that LPFs containing
34 CpreTM-TMD are recognized by 10E8 variants following their functional profile.
35 Furthermore, these formulations are immunogenic in rabbits, demonstrating their
36 capacity to engage with B-cell receptors.
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44 Third, we have altered the lipid composition of the membrane and evaluated its effect
45 on the antigenicity and immunogenicity of LPFs. It has been argued that a virus-like
46 membrane environment should be preserved in the conception of peptide vaccines
47 targeting the C-terminal region of MPER^{14, 36}. Thus, we used increasing concentrations
48 of Chol in the lipid mixtures in order to mimic the tight lipid packing of the viral
49 membrane⁴⁷. The antibody-based experiments revealed that C-MPER gets occluded in
50 the Chol-rich membranes, in line with the trend revealed by the immunogenicity assays.
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3 Consistent with this notion, recently published data indicate that the 10E8 epitope is
4 more accessible in cyclodextrin-treated virions, which purportedly contain lower
5 amounts of Chol⁶³.
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11 Given the crucial importance of the lipid composition in the development of a LPF
12 MPER vaccine, we further investigated the molecular basis for the Chol-induced 10E8
13 epitope occlusion. Our data demonstrate that the lipid bilayers containing the
14 reconstituted CpreTM-TMD peptide are stable in all compositions. However, the
15 increase in lipid packing induced by Chol appears to directly affect C-MPER helix
16 accommodation, provoking its unfolding and the loss of antigenicity.
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25 Under the assumption that to ensure reproducibility and lower cost, simple lipid
26 compositions would be preferred over complex lipid mixtures to manufacture liposome-
27 based vaccines^{14, 64}, in this work we have used a single lipid, Chol, to adjust lipid
28 packing. Nevertheless, other components of the HIV membrane such as sphingomyelin
29 (SPM) and aminophospholipids (phosphatidylserine/phosphatidylethanolamine)⁴⁶, can
30 increase membrane packing as determined by the Laurdan GP value⁴⁷. Thus, although
31 their ordering effects are less pronounced than those of Chol, in principle these lipids
32 could also interfere with MPER exposure at membrane surfaces. However, it is well
33 established that under certain conditions complex lipid mixtures that combine Chol with
34 low melting T^a phospholipids, and high melting T^a SPM, can undergo lateral
35 segregation generating Chol-rich (rigid) and Chol-depleted (fluid) domains in
36 membranes (see for instance ⁶⁵). Therefore, despite the high Chol content of the HIV
37 membrane and the presence of other lipids that enhance packing, it cannot be excluded
38 an effective recognition of the MPER epitope by antibodies and BCRs occurring within
39 the segregated fluid domains.
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3 Finally, we can speculate on whether the structures observed, and the effect of
4 Chol, provide some insight into the structure-function of Env. In this respect, a
5 crystal structure of the 6-helix bundle containing the full MPER sequence
6 supports the adoption of an extended conformation by MPER residues within
7 an Env fusion intermediate⁶⁶. Thus, we surmise that a tendency for
8 alternating the helical conformation of the MPER-TMD region with more flexible
9 and extended structures, might help completing the structural changes undergone by
10 the gp41 ectodomains upon fusion activation of the Env trimer (last step in Figure S1a).
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25 **CONCLUSION**

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28 Our goal in this work was to provide new pathways for the design of antiMPER
29 vaccines. Together, our results suggest that the reconstitution process stabilizes
30 a transmembrane CpreTM-TMD α -helix, exposing to solvent an accessible C-
31 MPER epitope. The increase of lipid packing induced by Chol appears to promote more
32 readily unfolding of the solvent-exposed and bulkiest section of the CpreTM-
33 TMD helix causing disruption of the C-MPER epitope. Thus, we infer that the increase
34 in Chol may force extrusion-extension of the C-MPER section to accommodate the
35 peptide chain, and induce the concomitant disorganization of the 10E8 epitope at
36 the membrane interface (Figure 6). In conclusion, our observations underpin the use of
37 CpreTM-TMD-based sequences in future designs of MPER-targeting vaccines ¹⁴,
38 but, contrary to common perception, they caution that reconstituted peptides aimed
39 to focus immune responses to the pan-neutralizing HIV-1 C-MPER sub-region
40 should be formulated in membranes devoid of Chol.
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METHODS

Reagents:

The peptide sequences derived from the gp41 MPER-TMD region, *KKK-NWFDITNWLWYIKLFIMIVGGLV-KK* (CpreTM) and *KKK-NWFDITNWLWYIKLFIMIVGGLVGLRIVFA-KKKK* (CpreTM-TMD) were produced by solid-phase synthesis using Fmoc chemistry as C-terminal carboxamides and purified by HPLC. 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phosphocholine (POPC), phosphatidic acid (egg, chicken) (PA), cholesterol (Chol), sphingomyelin (egg, chicken) (SM) and Lipid A detoxified (*Salmonella minnesota* R595) were purchased from Avanti Polar Lipids (Birmingham, AL, USA). N-(7-nitro-benz-2-oxa-1,3-diazol-4-yl)phosphatidylethanolamine (N-NBD-PE), N-(lissamine Rhodamine B sulfonyl)phosphatidylethanolamine (N-Rh-PE) and 6-dodecanoyl-2-dimethylaminonaphthalene (Laurdan) fluorescent probes were from Thermo Fisher Scientific (Waltham, Massachusetts, USA). Abberior STAR RED (KK114) was obtained from Abberior (Göttingen, Germany). Goat anti-Human IgG (Fab specific) – AP was obtained from Invitrogen (Carlsbad, California, USA) and goat anti-Rabbit IgG – AP from Thermo Fisher Scientific (Waltham, Massachusetts, USA).

Production of Fab 10E8 and its variants

Fab 10E8 antibody sequences was cloned in the plasmid pColaDuet and expressed in *Escherichia coli* T7-shuffle strain. Recombinant expression was induced at 18 °C overnight with 0.4 mM isopropyl-D-thiogalactopyranoside when the culture reached an optical density of 0.8. Cells were harvested and centrifuged at 8,000 × *g*, after which they were resuspended in a buffer containing 50 mM HEPES (pH 7.5), 500 mM NaCl,

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3 35 mM imidazole, DNase (Sigma-Aldrich, St. Louis, MO) and an EDTA-free protease
4 inhibitor mixture (Roche, Madrid, Spain). Cell lysis was performed using an Avestin
5 Emulsiflex C5 homogenizer. Cell debris was removed by centrifugation, and the
6 supernatant loaded onto a nickel-nitrilotriacetic acid (Ni-NTA) affinity column (GE
7 Healthcare, Chicago, Illinois, USA). Elution was performed with 500 mM imidazole,
8 and the fractions containing the His-tagged proteins were pooled, concentrated and
9 dialyzed against 50 mM sodium phosphate (pH 8.0), 300 mM NaCl, 1 mM DTT, and
10 0.3 mM EDTA in the presence of purified protease Tobacco etch virus ⁶⁷. Fabs were
11 separated from the cleaved peptides containing the His_{6x} tag by an additional step in a
12 Ni-nitrilotriacetic column. The flow-through fraction containing the antibody was
13 dialyzed overnight at 4 °C against sodium acetate (pH 5.6) supplemented with 10%
14 glycerol and subsequently loaded onto a MonoS ion exchange chromatography (IEC)
15 column (GE Healthcare, Chicago, Illinois, USA). Elution was carried out with a
16 gradient of potassium chloride and the fractions containing the purified Fab
17 concentrated and dialyzed against a buffer containing 10 mM sodium phosphate (pH
18 7.5), 150 mM NaCl, and 10% glycerol. For the preparation of mutant Fabs, the KOD-
19 Plus mutagenesis kit (Toyobo, Osaka, Japan) was employed following the instructions
20 of the manufacturer. For confocal microscopy experiments, position C216_{HC} of the fabs
21 was modified *in vitro* with a sulfhydryl-specific iodacetamide derivative of the KK114
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53 **Functional characterization of Fab 10E8 and its variants**

54 *Pseudovirus production*

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3 HIV-1 pseudoviruses were produced by transfection of human kidney HEK293T cells
4 with the full-length env clone JR-CSF (kindly provided by Jamie K. Scott and Naveed
5 Gulzar, Simon Fraser University, BC, Canada) using calcium phosphate. Cells were co-
6 transfected with vectors pWPXL-GFP and pCMV8.91, encoding a green fluorescent
7 protein and an env-deficient HIV-1 genome, respectively (provided by Patricia Villace,
8 CSIC, Madrid, Spain). For imaging experiments, pWPXL-GFP was replaced by
9 pEGFP.Vpr (NIH AIDS Reagent Program). After 24 h, the medium was replaced with
10 Optimem-Glutamax II (Invitrogen Ltd, Paisley, UK) without serum. Two days after
11 transfection, the pseudovirus particles were harvested, passed through 0.45 μm pore
12 sterile filters (Millex® HV, Millipore NV, Brussels, Belgium) and finally concentrated
13 by ultracentrifugation in a sucrose gradient at 24.000 rpm for 2h.
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29 *Super-resolution STED microscopy*

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32 EGFP.Vpr-labeled virions were immobilized on 0.1% poly-L-lysine coated coverslips
33 after 10 min incubation. Coverslips were then blocked with 2% BSA and antibodies
34 incubated in blocking buffer for 1 h at a concentration of 25 $\mu\text{g/ml}$ (ca. 0.5 μM). In the
35 case of unlabeled Fabs, the samples were incubated for an extra hour with donkey anti-
36 human STAR RED antibodies (1/200 dilution). Finally, samples were fixed with 2%
37 PFA and mounted in Mowiol//DABCO mounting medium.
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46 Imaging was performed using an Abberior STEDYCON system. STAR RED was
47 excited using a 640 nm pulsed laser line and depleted with using a 775 STED laser.
48 EGFP was excited with a 488 nm pulsed laser line. Emission was collected using
49 avalanche photodiodes. The emission filters were 650-700 nm for the super-resolved
50 STAR RED signal and 501-552 nm for the confocal EGFP signal. Pixel size was fixed
51 at 20 nm pixel, dwell time was 10 μs and line accumulation was set to 5.
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3 Only samples prepared in parallel and imaged within the same session were compared.
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5 To allow for comparison of independent experiments, intensity was normalized to the
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7 median 10E8 intensity after background noise subtraction. Image analysis was
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9 performed using the Python code developed previously^{35, 68} and available at this site
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11 (DOI: 10.5281/zenodo.1465920). The software automatically identified EGFP.Vpr
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13 positive particles using an intensity-maximum finding algorithm on a Gaussian
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15 smoothed image ($\sigma= 2.0$), and quantified the number of collected photons in a circular
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17 region of interest of 14 pixels (280 nm) in diameter. It performed the same
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19 quantification in a random region presenting no Vpr.EGFP signal, which was used as a
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21 reference background signal.
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26 27 *Cell entry assays*

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29 HIV entry was determined using TZM-bl target cells (AIDS Research and Reference
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31 Reagent Program, Division of AIDS, NIAID, NIH, contributed by J. Kappes). Serial
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33 dilutions of Fabs were incubated for 1.5 h at 37 °C with a 10–15% tissue culture
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35 infectious dose of pseudovirus. Samples were set up in duplicate in 96-well plates. After
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37 antibody-pseudovirus co-incubation, $1,1 \times 10^4$ target cells were added in the presence of
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39 30 $\mu\text{g/ml}$ DEAE-dextran (Sigma-Aldrich, St-Louis, MO). Neutralization levels after 72
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41 h were inferred from the reduction in the number of GFP positive cells as determined by
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43 flow cytometry using a BD FACSCalibur Flow Cytometer (BD Biosciences, San Jose,
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45 California, USA).
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52 53 **Liposome-peptide formulations**

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55 To prepare CpreTM-TMD containing LPFs, lipids and the CpreTM-TMD peptide were
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57 mixed in organic solvent prior to the production of the liposomes. Briefly, POPC, Chol
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3 (0, 20, 40 or 50 mol %) and PA (5 mol %) were dissolved in chloroform:methanol 1:2
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5 (vol:vol) and were mixed with CpreTM-TMD (dissolved in 100 % ethanol) at peptide-
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7 to-lipid molar ratio of 1:50. The mixture was dried under a N₂ stream and traces of
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9 organic solvents were removed by 2 h vacuum pumping. Subsequently, the dried lipid
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11 films were subjected to 2 h of gentle hydration with H₂O using a N₂ gas bubbler to
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13 facilitate the subsequent dispersion of the dried lipid-peptide film in PBS aqueous
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15 buffer. Next, the multilamellar vesicles were bath sonicated (1 h, 55 °C) and subjected
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17 to 15 freeze and thaw cycles to obtain unilamellar vesicles. Chol concentration of
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19 liposome suspensions was determined by the cholesterol oxidase/peroxidase method
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21 (BioSystems, Barcelona, Spain), and found to be within the experimental error.
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27 **Rabbit immunization and response analysis by ELISA**

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30 New Zealand White rabbits were immunized at the antibody production service from the
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32 CID-CSIC (Barcelona, Spain). Liposome-based formulations were prepared following
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34 the methods described above including 0.25 mol % Lipid A as adjuvant ⁶⁴ and were
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36 lyophilized. Two rabbits were inoculated intradermally at multiple sites on day 0 with 1
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38 ml of each LPF sample reconstituted in pure water, which contained 0.4 mg peptide.
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40 Subsequent boosting injections, consisted of 1 ml of the reconstituted liposome
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42 formulation containing 0.3 mg peptide on day 21, while 0.2 mg of liposomal peptide
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44 were injected on day 42.
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50 *Enzyme-linked immunosorbent assay (ELISA)*

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53 LPFs were dissolved in phosphate-buffered saline (PBS) at a concentration of 500 µM
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55 and 1:50 CpreTM-TMD:lipid (mol:mol ratio) and immobilized (100 µl/well) overnight
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57 onto C96 Maxisorp microplate wells (Nunc, Denmark). The plates were blocked for 2 h
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3 with 3 % (w/v) BSA in PBS and incubated with either the Fabs or rabbit sera for 4
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5 hours. The binding of the Fabs or sera IgGs was detected by incubation for 50 min with
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7 1:1000 dilution of alkaline phosphatase-conjugated goat anti-human IgG F(ab)₂
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9 (Invitrogen, Carlsbad, CA, USA) or goat anti-Rabbit IgG (Thermo Fisher Scientific
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11 (Waltham, MA, USA) respectively, which then catalyzed a color reaction for 30 min
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13 with 1 mg/mL p-nitrophenyl phosphate substrate (VWR International, Radnor,
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15 Pensilvania, USA) in 0.1 M glycine, 1 mM MgCl₂, 1mM ZnCl₂, pH 10.4, that could be
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17 measured by absorbance at a wavelength of 405 nm in a Synergy HT microplate reader
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19 (Bio-TEK Instruments Inc., VT, USA). The plates were extensively washed with PBS
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21 after each step.
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29 **Single-vesicle assays for membrane stability**

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32 Giant unilamellar vesicles were produced by spontaneous swelling as described by
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34 Velasco-Olmo et al. ⁶⁹ In brief, 0.125 mg lipid was co-dissolved in 100 μ L
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36 CHCl₃:CH₃OH (9:1) with the fluorescent probes Laurdan (1 mol %) or NBD-PE (2 mol
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38 %). When required, CpreTM-TMD peptide (dissolved in 100 % ethanol) was included
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40 in organic phase at 1:50 peptide-to-lipid ratio. The probe-containing lipid or lipid-
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42 peptide mixture was introduced in a vacuum desiccator for 1 h to remove the organic
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44 solvent and the desiccated lipid was hydrated with Milli-Q water for 1 h at temperatures
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46 above the transition temperature of the mixture (typically 55° C). 5 μ L silica beads (40
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48 μ m) were then mixed with 20 μ L of the MLV suspension, separated in 3.5 μ L drops on
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50 a teflon film and vacuum dried for 1h. Dried beads covered with lipid were collected
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52 and transferred to an 85 g/L sucrose buffer in order to induce spontaneous swelling of
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54 GUVs. Finally vesicles were transferred to the observation dish in an isosmotic 10 mM
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56 Hepes, 150 mM KCl (pH 7.4) buffer.
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3 For binding experiments, NBD-labeled GUVs with increasing concentrations of
4 cholesterol and with or without the CpreTM-TMD peptide (1:50 peptide-to-lipid molar
5 ratio) were used. The GUVs were added to a bovine serum albumin (BSA)-blocked
6 microscope chamber that already included 250 nM of 10E8-based Fabs conjugated with
7 the KK114 probe at residue C216_{HC}, and were incubated for 15 min prior to imaging.
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12 For GUV-LUV heterotypic fusion experiments, NBD-labeled POPC:Chol:SM (2:2:1
13 mol:mol) GUVs devoid of peptide were added to a suspension of Rho-labeled LUV
14 previously incubated with the CpreTM peptide or to a suspension of Rho-LPFs bearing
15 CpreTM-TMD, both at 1:50 peptide-to-lipid molar ratio, and were incubated for 15 min
16 prior to imaging.
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20 For GUV permeabilization assays, NBD-labeled CpreTM-TMD-bearing GUVs were
21 added to a BSA-blocked microscope chamber that already included the unconjugated
22 and soluble KK114 dye, and were incubated for 15 min prior to imaging.
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26 27 28 *Confocal microscopy*

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30 Images were acquired on an inverted confocal fluorescence microscope (Nikon Eclipse
31 TE-2000, Nikon, Nikon Instruments, Tokyo, Japan). NBD-stained GUVs, Rho-labeled
32 LUVs and Fabs conjugated with the KK114 probe were excited at 476 nm, 514 nm and
33 637 nm, respectively. For GUV-LUV heterotypic fusion experiments, the fluorescence
34 signal was collected into two different channels with band pass filters of 515/30 nm, and
35 590/94 nm. For binding and permeabilization experiments the band pass filters used
36 were 515/30 and Long Pass 650 nm. The objective used was a 63X oleo immersion with
37 a numerical aperture (NA) of 1.2.
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41 Relative extents of Fab-GUV binding or LUV-GUV fusion were obtained by measuring
42 the fluorescence intensity of KK114 or Rhodamine, respectively, along the equatorial
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3 plane of the GUV images. Extents of permeabilization were calculated for each vesicle
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5 after 15 min incubation with KK114 following equation 1,
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$$8 \quad \text{Permeabilization (\%)} = \frac{F_{\text{inside}}}{F_{\text{outside}}} \times 100 \quad \text{Eq. 1}$$

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15 where F_{inside} and F_{outside} are the average of KK114 fluorescence intensities inside and
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17 outside a GUV, respectively. Fluorescence emission analyses were carried out with
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19 ImageJ software (rsb.info.nih.gov/ij/).
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22 23 *Membrane packing analysis by Multiphoton Fluorescence Microscopy*

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26 Images were acquired on a Leica TCS SP5 II microscope (Leica Microsystems GmbH,
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28 Wetzlar, Germany). For multiphoton excitation, the sample was illuminated with a 780
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30 nm beam from a femtosecond-pulsed titanium-sapphire Mai-Tai Deepsee (Spectra-
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32 Physics, Berlin, Germany) laser. GUVs were imaged through a $\times 63$ water-immersion
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34 objective (NA=1.2) and 512x512 pixel images were acquired at 400 Hz per scanning
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36 line. Fluorescence emission was collected by non-descanned (NDD) hybrid detectors, as
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38 they offer higher sensitivity compared to photomultipliers. NDD 1 collected the blue
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40 edge of the emission spectrum at 435 ± 20 nm and NDD 2 collected the red edge at 500
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42 ± 10 nm. For Generalized Polarization (GP) measurements unilamellar GUVs were
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44 selected and imaged at the equatorial plane to avoid photoselection.
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50 GP values were calculated using in-house developed software based on MATLAB
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52 (MathWorks, MA, USA) as described in our previous papers^{24, 65}. After smoothing the
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54 images with a 2-pixel averaging circular filter and thresholding the intensity, GP values
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56 were calculated for every pixel on the image following equation 2,
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$$GP = \frac{I_B - G \times I_R}{I_B R + G \times I} \quad Eq. 2$$

where I_B is the intensity collected by NDD 1, I_R the intensity collected by NDD 2 and G is the factor that accounts for the relative sensitivity of the two channels, calibrated with 5 μ M Laurdan solution in pure DMSO⁶⁵. The mean GP value for each lipid mixture was calculated after imaging and analyzing at least 15 GUVs in each independent experiment.

Infrared spectroscopy

Infrared spectra were recorded in a Bruker Tensor 27 spectrometer equipped with a mercury-cadmium-telluride detector using a Peltier-based temperature controller (TempCon, BioTools Inc., Wauconda, IL) with calcium fluoride cells (BioCell, BioTools Inc., Wauconda, IL). LPFs were lyophilized and subsequently prepared at 3 mg/mL in D₂O buffer (PBS). A 25 μ L sample aliquot was deposited on a cell that was sealed with a second cell. Reference windows without peptide were prepared similarly. Typically 1000 scans were collected for each background and sample, and the spectra were obtained with a nominal resolution of 2 cm^{-1} . Data treatment and band decomposition of the original amide I have been described elsewhere⁵².

ANCILLARY INFORMATION

Supporting Information Available

Supporting Methods: description of the liposome-flotation assay. Supporting Figures S1-S6: This material includes a diagram to explain the strategy followed to focus immune responses to C-MPER epitope (Fig. S1), single virion-antibody binding data obtained from STED measurements (Fig. S2), determination of peptide incorporation to liposome vaccines through flotation experiments (Fig. S3), size polydispersity distributions of LPFs (Fig. S4), GUV-antibody binding data (Fig. S5) and secondary structure composition of CpreTM-TMD as a function of the Chol content in membranes (Fig. S6). Supporting bibliography

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Author Contributions

B.A. and J.L.N. designed research; J.T, I.DA, P.C., S.I., E.R., E.L., and B.A., performed research; J.T., I.DA, P.C., E.R., E.L., C.E., J.L.R.A., B.A. and J.L.N. analyzed data; and B.A. and J.L.N. wrote the paper with input from all authors.

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21 **Abbreviations Used:** bnAb, broadly neutralizing antibody; GP, General Polarization;
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23 GUV, Giant Unilamellar Vesicle; LPF, Liposome-peptide formulation; LUV, Large
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25 Unilamellar Vesicle; MPER, Membrane-Proximal External Region; C-MPER,
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27 Carboxy-terminal subregion of MPER; TMD, Transmembrane Domain.
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6 **neutralizing HIV-1 epitope**
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